



## **Psoas muscle area and quality are independent predictors of survival in patients treated for abdominal aortic aneurysms**

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1 **Psoas muscle area and quality are independent predictors of survival in patients treated for**  
2 **abdominal aortic aneurysms**

3  
4 Iisa Lindström, MS <sup>a</sup>, Niina Khan, MD <sup>b</sup>, Teemu Vänttinen, MD, PhD <sup>b</sup>, Mikko Peltokangas  
5 MSc(tech)<sup>c</sup>, Niko Sillanpää, MD, PhD <sup>d\*</sup>, Niku Oksala, MD, PhD, DSc <sup>a,b,e\*</sup>

6  
7 <sup>a</sup> Faculty of Medicine and Life Sciences, University of Tampere, FI-33014, Tampere, Finland

8 <sup>b</sup> Division of Vascular Surgery, Department of Surgery, Tampere University Hospital, PO BOX 2000  
9 FI-33521 Tampere, Finland

10 <sup>c</sup> BioMediTech Institute and Faculty of Biomedical Sciences and Engineering, Tampere University  
11 of Technology, Tampere, Finland

12 <sup>d</sup> Medical Imaging Center, Tampere University Hospital, PO BOX 2000, FI-33521, Tampere, Finland

13 <sup>e</sup> Finnish Cardiovascular Research Center, Tampere, Finland

14  
15 \* These authors share senior authorship

16  
17 Corresponding author: Professor N. Oksala, Faculty of Medicine and Life Sciences, University of  
18 Tampere, FI-33014, Tampere, Finland. Email address: niku.oksala@professori.fi

19  
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26

27 **ABSTRACT**

28 **Background:** Sarcopenia is associated with mortality after abdominal aortic aneurysm (AAA) repair.  
29 The reliability of computed tomography (CT) core muscle areas and quality i.e. densities and their  
30 association with postoperative survival in patients undergoing AAA treatment were retrospectively  
31 studied.

32 **Methods:** Psoas and multifidus areas (PMA, MFA) and densities (PMD, MFD) were measured from  
33 CT images and analysed to lean values. Results were standardized by z-scoring. Measurement  
34 reliability was ascertained using intraclass correlation coefficient (ICC) analysis (three independent  
35 observers). Clinical data was collected from an institutional database and the hospital's patient record  
36 database.

37 **Results:** The study included 301 patients (89% male, mean age 74.4 years, endovascular treatment  
38 73.1%, rupture 7.6%). Median duration of follow-up was 2.70 (IQR 3.54) years and mortality 31.2%.  
39 Age, female gender, and BMI were associated with PMA, PMD and lean psoas muscle area (LPMA).  
40 L3 left PMD, total psoas muscle density (TPMD), right and left LPMA, lean total psoas muscle area  
41 (LTPMA) and L2 right LPMA and LTPMA (HR 0.74-0.78 per one standard deviation,  $P < .05$  –  $P < .01$ )  
42 were independently associated with improved survival in multivariable analysis.

43 **Conclusions:** L2-L3 PMD and LPMA are reliable, feasible and independent predictors of mortality  
44 in patients treated for AAA. For every standard deviation increase in these standardized z-score  
45 muscle parameters, there was a 22% - 26% decrease in the probability of death during follow-up.

46 **Keywords:** Abdominal Aortic Aneurysm, CT volumetry, Paraspinal muscle

47

48 **INTRODUCTION**

49

50 Surgical procedures for abdominal aortic aneurysms (AAA) are high-risk interventions with  
51 considerable postoperative mortality. Survival is influenced by several factors such as urgency of  
52 operation, age, sex, and comorbidities like renal insufficiency, congestive heart failure, and chronic  
53 obstructive pulmonary disease.<sup>1-5</sup> The effect of treatment modality, open versus endovascular aortic  
54 repair (EVAR), has been somewhat controversial but EVAR has shown early survival benefit over  
55 open surgery in elective surgery and better long-term survival, cost-effectiveness and quality of life  
56 when treating ruptured aneurysms in the emergency setting.<sup>6-12</sup> Development of surgical and  
57 anaesthesiologic techniques along with aging of the population has led to vascular surgical patient  
58 material becoming more challenging which in turn emphasises the need for improved methods of risk  
59 prediction in order to optimise patient safety, operative results, and cost-effectiveness.

60

61 Frailty, the age-associated decline in overall physiologic reserve and function, is associated with  
62 subclinical cardiovascular disease and appears to be superior to conventional anaesthesiologic or  
63 surgical risk scores in estimating postoperative survival.<sup>13-16</sup> Muscle mass measures are one way of  
64 assessing frailty and skeletal muscle depletion referred to as sarcopenia has been demonstrated as an  
65 independent predictor of postoperative mortality.<sup>16-21</sup> Core muscle mass estimates have been found  
66 to be associated with postoperative survival even in patients undergoing elective AAA repair and  
67 sarcopenia has been noted to be associated with worse survival after elective EVAR and open  
68 surgery.<sup>22-26</sup> The methods for estimating both frailty and sarcopenia vary and the current challenge  
69 lies in defining an approach that is objective, reproducible, and convenient for the clinician without  
70 adding costs.<sup>13,16</sup> Furthermore, there is a need for evidence on the effect of sarcopenia as an indicator  
71 of muscle quality on survival of AAA patients undergoing invasive treatment including also urgent  
72 and emergency cases. Psoas muscle area (PMA) can be applied as a quantitative method of estimating  
73 core muscle mass and sarcopenia and it correlates with postoperative complications and mortality.<sup>23,27</sup>  
74 It should be noted, that PMA correlates negatively with age and positively with weight.<sup>23</sup> Similarly,

75 paraspinal muscle area has been used in core muscle evaluation and is associated with postoperative  
76 survival.<sup>28,29</sup> Taken together, previous evidence on the effect of sarcopenia on survival of AAA  
77 patients is limited to elective patients and on PMA while data on reproducibility of the measurement,  
78 the value of other muscles and muscle quality as reflected by density is not available.

79

80 The purpose of this study was, firstly, to ascertain the reproducibility of core muscle area and quality  
81 i.e. density measurement from computed tomography (CT) scans of AAA patients by three  
82 independent observers and select the most consistent parameters. Secondly, the study sought to  
83 determine the association of sarcopenia represented by these density and lean area parameters with  
84 postoperative mortality in a cohort of patients treated for AAA with open surgery or EVAR electively  
85 or in an urgent or emergency setting. To explore more clinical association between psoas area and  
86 quality we performed muscle parameters standardization by z-scoring.

87

88

89

## 90 **METHODS**

91

### 92 **Patients**

93 For this study a total of 301 patients were randomly selected from a larger cohort of patients (n=959)  
94 undergoing AAA treatment in the Tampere University Hospital (TAUH) vascular clinic between  
95 2001 and 2014. The data was collected from a prospectively constructed institutional database and  
96 TAUH patient record database. The clinic's protocol of preoperative assessment entailed aortic  
97 imaging with contrast-enhanced CT for each patient. Additional CT imaging was conducted  
98 postoperatively as part of the follow-up at one month and two years in patients who underwent EVAR.  
99 The treatment modality, open or endovascular surgery, was selected by the treating vascular surgeon  
100 often in collaboration with an interventional radiologist in a multidisciplinary meeting. The study  
101 adhered to the ethical principles of the Declaration of Helsinki and was approved by Pirkanmaa  
102 Hospital District Science Center Approval. Due to the nature of the study no informed patient consent  
103 was required or obtained. A total of 100 patients were first evaluated and it was found that a 6-10%  
104 change in parameter values caused a significant difference in mortality. It was therefore decided to  
105 measure 201 additional patients yielding a sufficient sample. Patients without available CT imaging  
106 of the abdominal area between 90 days before and 30 days after the operation with 0.63-3.00 mm  
107 slice thickness were excluded. The excluded patients had less dyslipidaemia (28.9 % vs. 43.9%,  
108  $P<.001$ ) and coronary artery disease (CAD) (41.5 % vs. 50,8 %,  $P=0.007$ ), but no significant  
109 differences were observed in other demographic parameters.

110

### 111 **Imaging parameters**

112 CT scans were obtained using two different multidetector scanners: General Electric LightSpeed 16-  
113 row (GE Healthcare, Milwaukee, WI, USA) and Philips Brilliance 64-row (Philips, Cleveland, OH,  
114 USA). Scanners were in equal use and patients were not selected to a certain scanner. Abdominal  
115 aortic CT imaging was performed using the following parameters: 120 kV, 250 mAs, collimation  
116  $64 \times 0.625$  mm (64-row) or 120 kV, Auto MA (150-350 mAs), collimation  $16 \times 1.25$  mm (16-row).

117 Contiguous slices were reconstructed to the thickness of 1-3 mm in the whole scanning range. The  
118 contrast agent (Xenetix 350 mgI/mL, Aulnay-sous-Bois, France) was administered through an  
119 antecubital 18-G cannula using a double-piston power injector with a flow rate of 3 mL/s using 100  
120 mL of contrast agent followed by a 40-mL saline flush. Real-time bolus tracking was used and the  
121 acquisition was triggered when the contrast agent opacified the full diameter of the thoracoabdominal  
122 aorta. The acquisition was performed during deep-inspiration breath-hold.

123

#### 124 **Image analysis, variables, and measurements**

125 The CT images were reviewed using dedicated medical imaging workstations (Carestream Vue PACS  
126 viewer version 11.4.0.1253, Rochester, NY, USA). Density and area measurements were performed  
127 from contrast-enhanced arterial phase images and axial slices of 0.63-3.00 mm thickness were used.  
128 The distances between the transverse processes were measured from sagittal reformats reconstructed  
129 with the multiplanar reformat (MPR) feature of the viewer software. Preferentially, the preoperative  
130 aortic imaging study was utilised. When preoperative images with the desired slice thickness were  
131 unavailable the one-month or earlier follow-up aortic CT was evaluated (21.9% of cases). Of these,  
132 90.9% were elective and 95.5% were EVAR.

133

134 A test sample of 27 patients was first randomly selected and evaluated independently by three  
135 clinicians: a radiologist (10 years of experience), a vascular surgeon (15 years of experience), and a  
136 junior doctor who had been previously given appropriate instructions. The purpose was to extensively  
137 test the reliability and prognostic value of repeated measurement of the same muscle area in the  
138 clinical work. All evaluators were blinded to the patients' outcome and test patients' characteristics  
139 did not significantly differ from the remaining patients. The remaining patients were evaluated by a  
140 single interpreter based on observations from the test sample. The measurements were performed on  
141 both sides at four vertebral levels: L2, L3, L4, and L5. A representative axial slice for each vertebral  
142 level was chosen at the level of origin of the transverse processes. Regions of interest (ROIs) that  
143 separately outlined the psoas and multifidus muscles on both sides were carefully drawn with a free-

144 hand tool that subsequently produced a report giving the cross-sectional area outlined by the ROI and  
145 the mean density in Hounsfield Units (HUs) along with standard deviation (SD) (Figures 1, 2). The  
146 idea was to isolate the muscle according to the anatomical boundaries in axial images. Free-hand  
147 selection of ROI measured the area and mean density.

148

149 Total muscle areas were formed by adding the right and left muscle areas and total muscle densities  
150 were calculated as means on each sides at the same vertebral level. Distances between vertebrae were  
151 measured between the caudal margins of the transverse processes in the sagittal plane of the mid part  
152 of the transverse process of the more cranial vertebra. The side with longer distance was chosen for  
153 measurements if there was a visible difference. After confirmation of reproducibility which ranged  
154 from fair to excellent being fair in two type of CT measurements, the remaining 274 patients were  
155 evaluated by a single interpreter based on the observations gathered from the test sample. Density  
156 thresholds for tissue characterizations were set as follows: 20-80 HU normal muscle, 1-19 HU lower  
157 density muscle, 0 HU water, -1 to -29 HU fatty muscle, and -30 to -50 HU fatty connective tissue.  
158 Contrast between psoas muscle tissue and adipose tissue is considerable as a consequence of  
159 prominent fascia and muscle measurements can be done as a semi-automated procedure. Isolation  
160 using HU-based segmentation would not work in a muscle with fatty streaks and subfascial fat  
161 because the region growing algorithm would not be able to discriminate the intramuscular fat from  
162 the surrounding fat. Inside the free-hand ROI, HU-based segmentation into fat and muscle would be  
163 possible. However, the density-area product was elected in line with previous reports.<sup>23,29</sup>

164

165 Lean muscle area was estimated by the product of total muscle area with average density ( $\text{cm}^2 \times \text{HU}$ ).  
166 This value was scored as zero if the average density was below 0 HU. Lean muscle area was estimated  
167 by the product of total muscle area with average density ( $\text{cm}^2 \times \text{HU}$ ) which enabled accounting for  
168 both muscle area and density on the same variable. Lean muscle area was scored as zero if the average  
169 density was below 0 HU. The study centre's medical imaging workstation was not able to directly  
170 measure lean variables. The psoas muscle volume was modelled for calculations as a 3D truncated



171 cone, where distance between vertebrae was the height of the cone and total muscle area was the area  
172 of the base of the cone.

173

#### 174 **Statistical analysis**

175 The statistical software used for analyses was SPSS 24 for Mac OS X. Intraclass correlation  
176 coefficient analysis (ICC) was applied to ascertain reliability, i.e. interobserver variability of the  
177 parameters (areas, densities and distances) measured by the three independent observers. Not all the  
178 observers traced the region of interest twice so intraobserver variables are not shown. The two-way  
179 random single measurement model was selected and both consistency and absolute agreement were  
180 calculated along with 95% confidence intervals.<sup>30</sup> ICC was rated as poor (<0.40), fair (0.40-0.59),  
181 good (0.60-0.74) or excellent (0.75-1.00). A test sample size of approximately 10% of the whole  
182 sample (>20 patients) is typical in testing the functionality of a study as the measurement error  
183 decreases significantly at this threshold. In the present study, post-hoc statistical power estimates  
184 were calculated for the ICC values as assurance probabilities as proposed by Zou et al.<sup>31</sup> The  
185 assurance probability is alternative to power analysis when ICC results are the primary outcome and  
186 it indicates the probability that the lower limit of the confidence interval is no less than the obtained  
187 value. In the present study, assurance probabilities results were excellent (0.80-0.92) in almost all of  
188 the statistically significant measurements indicating that the 27-patient test sample applied was  
189 sufficient.

190

191 The distributions of the measured variables were visualised using histograms and analysed for  
192 normality using Levene's test. Predictors of survival were analysed using Cox regression first in  
193 univariable analyses and testing the proportional hazards assumption by log-minus-log plots, and  
194 consequently in a multivariable model including parameters with  $P < .1$  in univariable analysis as  
195 covariates. Muscle parameters were entered as continuous variables to the Cox regression analysis.  
196 Multivariable regression was adjusted as covariates for age, ruptured AAA, smoking, previous stroke  
197 or transient ischemic attack (TIA), creatinine-level, ASA-score, statin and anticoagulant medication.

198 Multivariable analyses were also calculated by standardized z-scoring variables and analyses were  
199 adjusted for the same variables. Statistical significance was set at  $P < .05$ .

200

201

202

## 203 **RESULTS**

204

### 205 **Patient demographics**

206 The final study population consisted of 301 patients treated for AAA in TAUH between 2001 and  
207 2014. The demographic data, risk factors, procedural variables, and medication are presented in Table  
208 1. There were no patients with missing data. The majority of patients were male, presented with  
209 coronary artery disease (CAD) and hypertension, underwent an elective procedure, received EVAR,  
210 were classified as ASA3, and had statin medication.

211

### 212 **Reproducibility of the CT measurements**

213 The distance between L2 and L3 vertebrae was clearly the most consistently measured one among  
214 the different vertebral levels based on ICC analysis (consistency 0.599, 95% CI 0.25-0.86; absolute  
215 agreement 0.588, 95% CI 0.25-0.85; Table 2). Thus, muscle volume and density measurements were  
216 performed on these two levels. The measurements demonstrated fair to excellent reliabilities, mostly  
217 in the range of good reproducibility (Table 2). Consistency was 0.535-0.686 and absolute agreement  
218 0.446-0.585 for PMA at L2, and 0.672-0.720 and 0.640-0.676 at L3, respectively. For PMD  
219 consistency was 0.769-0.816 and absolute agreement 0.776-0.793 at L2 level and 0.691-0.765 and  
220 0.693-0.778, correspondingly, at L3 level. PMAs measured at these levels had moderate to high  
221 correlation to the areas of the multifidus muscles at the same levels based on Pearson R (L2: R=0.719,  
222 P<.01, L3: R=0.469, P<.05). A similar finding was observed when densities were compared (L2:  
223 R=0.512, P<.01, L3: R=0.654, P<.01).

224

### 225 **Association of age, gender, and BMI with the CT-measurements**

226 Clinical features were similar between men and women in terms of demographics, risk factors and  
227 procedural variables, but men used significantly more antihypertensive medication (P=.04). When  
228 comparing sides (dx vs. sin), the left-sided parameters were significantly higher: L2 PMA ( $5.2 \pm 2.0$   
229 vs.  $5.5 \pm 1.9$  cm<sup>2</sup>), L2 PMD ( $29.3 \pm 12.6$  vs.  $31.7 \pm 11.8$  HU), L3 PMA ( $8.2 \pm 2.6$  vs.  $8.5 \pm 2.5$  cm<sup>2</sup>),

230 L3 PMD ( $32.0 \pm 12.0$  vs.  $33.4 \pm 11.3$  HU), L2 lean PMA ( $155.2 \pm 93.1$  vs.  $175.4 \pm 93.1$  cm<sup>2</sup> x HU),  
231 L3 lean PMA ( $253.3 \pm 138.2$  vs.  $287.8 \pm 135.9$  cm<sup>2</sup> x HU) showed significant differences ( $P < .01$  for  
232 all).

233

234 Table 3 presents the actual median values of measured muscle areas and densities. Furthermore, the  
235 effects of age, gender, and BMI are presented on the measured CT parameters. Aging had an overall  
236 inverse effect on psoas muscle area, density, lean area and volume, and lean volume. Female gender  
237 was associated with decreased psoas muscle area, lean area, density and volume, and lean volume.  
238 Finally, BMI was associated with increased psoas muscle area and volume (Table 3).

239

#### 240 **Association of CT measurements with mortality**

241 The follow-up lasted until April 2015 with the median duration of follow-up being 2.70 (IQR 3.54)  
242 years. Ninety-four (31.2%) patients died and none were lost during follow-up. Parameters with a  
243 tendency to predict survival in univariable analyses (Supplementary table 1) were checked by log-  
244 minus-log plots to confirm proportional hazards assumption and were thereafter incorporated into the  
245 multivariable analysis (Supplementary table 2). Results were also confirmed by further adjusting the  
246 multivariable model with BMI and gender known to associate with PMA and the results remained  
247 the same (Supplementary table 3). To explore more clinical association between psoas muscle density  
248 or lean area and outcome, the multivariable analysis after muscle parameters standardization by z-  
249 scoring was performed (Table 4). L3 left side PMD and total psoas muscle density (TMPD), L3 right  
250 and left lean psoas muscle area (LPMA), L3 lean total psoas muscle area (LTPMA) and L2 right  
251 LPMA and LTPMA (HR 0.74-0.78 per 10 HU) per one standard deviation ( $P < .05$  –  $P < .01$ ) were  
252 independently associated with improved survival in multivariable analysis. The most effective muscle  
253 parameter was L3 LTPMA, for which for every standard deviation increase means 26% decrease in  
254 the probability of death during follow-up. Z-scoring decreased muscle parameters skewing compared  
255 to authentic muscle parameters (Supplementary table 2). Further adjustment of the model with  
256 operative approach (EVAR vs. open repair) or urgency (emergency vs. elective) did not have any

257 effect on the results. Furthermore, multivariable analysis was performed also with z-scored muscle  
258 parameters and after exclusion of ruptured AAA-patients. In these analyses, L3 TPMD (HR 0.68-  
259 1.01) and L2 LTPMA (HR 0.60-1.01) demonstrated slightly decreased significance, but the most  
260 consistently associated muscle parameter L3 LTPMA strengthened and every standard deviation  
261 increase was associated with a 29% decrease in the probability of death. Ruptured AAA-patients did  
262 not have statistically significant to the results. The effect of pre-postoperative imaging was also tested  
263 by univariable Cox regression analysis and no association with survival was found.

264

265

266 **DISCUSSION**

267

268 Muscle size and quality are significant predictors of postoperative mortality. However, the optimal  
269 method for estimating these in a reliable and convenient way is yet to be determined and the evidence  
270 regarding vascular surgical patients remains limited. The present study demonstrated the association  
271 of muscle quality with mortality in patients treated for AAA in 1-5-year follow-up using PMD, PMA,  
272 and lean PMA at the level of the L2 and L3 vertebrae as markers that can be reliably and swiftly  
273 measured from CT scans. In the present study, the strongest cut off-value affecting prognosis was a  
274 one standard deviation increase in the psoas muscle lean area bilaterally at the L3 level. Specifically,  
275 at a cut-off value for total psoas lean area of 269.4 cm<sup>2</sup> or greater at the L3 level was associated with  
276 a 26% decrease in the probability of death during follow-up. Results can be generalized in the clinical  
277 work, when the muscle standardized deviation of the local patient series is measured and known.  
278 Other research has studied the association between muscle area and patient outcome, but in the  
279 present study, attention was paid also to lean values including both muscle area and density (cm<sup>2</sup> x  
280 HU). Preoperative CT images within 90 days before the operation were preferred, but if these were  
281 unavailable the one-month or earlier postoperative images were used. It was verified that the timing  
282 of CT imaging was not significantly associated with survival. It was additionally ascertained that  
283 PMD is negatively associated with age and female gender in patients undergoing AAA repair.

284

285 The fair to excellent reproducibility of PMA and PMD measurements at L2-L3 vertebral levels as  
286 shown by ICC analysis is in line with previous studies and suggests that these parameters can be  
287 reproducibly estimated from routine preoperative CT scans.<sup>32,33</sup> PMA and PMD correlated with MFA  
288 and MFD at L2-L3 levels. Reproducibility of multifidus muscles areas were tested by ICC at the same  
289 vertebral level, but the results were weaker. These findings most likely result from the challenges of  
290 outlining the ROIs of the multifidus muscles if there is no perceptible fascia. Apart from left lean  
291 muscle volumes the study patients presented with greater muscle areas and densities on the left side  
292 compared to the right. Previously, PMA has been found to be greater on the dominant side in a study

293 cohort of healthy males.<sup>34</sup> A study investigating the potential causes of paraspinal muscle asymmetry  
294 in men found only some inconsistent associations with muscle laterality, including handedness.<sup>35</sup>  
295 Whether the asymmetry noted in the present study was influenced by the AAA via different  
296 mechanisms remains to be elucidated. With regards to factors associated with the investigated muscle  
297 parameters, the significant inverse association of age with PMA and PMD fits well to the very  
298 definition of frailty and further supports the use of muscle mass and quality estimates as methods of  
299 frailty assessment.<sup>13,14,23,36</sup> The tendency of women towards lower PMA, PMD, and lean muscle  
300 volume compared to men is supported by preceding evidence.<sup>37-39</sup> The present study found that in  
301 addition to age, BMI is associated with increased PMA and total psoas muscle area, which is seconded  
302 by current literature.<sup>23</sup> A similar correlation has been noted before in lung cancer patients undergoing  
303 pneumonectomy.<sup>21</sup> The multivariable models were adjusted with age, gender, BMI, operative  
304 approach and urgency, and with all significant factors found in univariable analyses but these  
305 adjustments had no effect on the association of psoas muscle parameters with survival which further  
306 confirms the independent role of these parameters as predictors of mortality.

307

308 Previous work on the effect of sarcopenia on survival in vascular surgical patients includes a study  
309 by Canvasser et al<sup>29</sup>, which stated that paraspinal muscle area at Th12 level measured from  
310 preoperative abdominal CT scans is associated with postoperative 1 year mortality. Paraspinal muscle  
311 area measurements were used as the group found them more easily attainable from routine imaging  
312 compared to psoas muscle measurements for a larger group of surgical patients. Additionally,  
313 paraspinal muscle area was noted to correlate well with total psoas muscle area at L4 level. Despite  
314 the substantial study cohort (n=1309) the percentage of vascular surgical patients was only 13.5, the  
315 study excluded outpatients and those subjected to emergency surgeries, and did not provide data on  
316 AAA patients. In comparison, the study cohort in the present study is more homogenous entailing  
317 only patients subjected to AAA repair, includes both elective and emergency cases, patient data is  
318 comprehensive, and the follow-up is longer (2.70 years, IQR 3.54). Previous studies in AAA patients  
319 have a comparable follow-up and are in line with the present findings thus consolidating evidence on

320 the predictive value of PMA in postoperative survival of elective patients (n=149) treated mainly with  
321 EVAR (85%; HR 0.86 per cm<sup>2</sup>)<sup>23</sup>, elective patients (n=137) treated mainly with EVAR (96%)<sup>26</sup> and  
322 elective patients (n=262) treated with open repair<sup>22</sup>. In more recent papers, Newton et al<sup>24</sup> found  
323 sarcopenia to be associated with worse survival in patients (n=135) undergoing elective EVAR (OR  
324 3.9, P=0.027) and Thurston et al<sup>25</sup> presented similar findings in an elective all male EVAR cohort (JR  
325 2.37, P=0.011). Shah et al<sup>26</sup> included postoperative CT images within 3 months after operation in  
326 case of missing preoperative images in 12% of cases and the group discovered reduced left PMA at  
327 L4 level to be independently associated with mortality which is supported by the results of the present  
328 study.<sup>26</sup> Contrary to other works Indrakusuma et al<sup>40</sup> did not find an association between low PMA  
329 at the level of L3 and survival in AAA patient. The study of 228 elective, asymptomatic infrarenal  
330 AAA patients only 124 underwent AAA repair and 62% of 124 patients were treated by EVAR. Their  
331 study did not include patients who had symptomatic pain or ruptured AAA and multivariable analysis  
332 of significant univariable parameters and overall survival was not presented. Advantageously, the  
333 present study adds on previous knowledge by providing data on the value of PMD and lean PMA  
334 parameters, indicating that in addition to area, also muscle quality has predictive value. Furthermore,  
335 the present study applied both authentic and z-scored values to control for skewing and to enhance  
336 more clinical importance to the results. Low muscle size and density are potential variables when  
337 considering the fitness of a patient for operation, particularly for A high risk operation.

338

339 The results presented in this paper should be interpreted in the context of a single-centre retrospective  
340 study. The vascular registry used is, however, constructed prospectively and annually audited.  
341 Furthermore, patients treated before 2005 were mainly excluded from the study since CT slice  
342 thickness of 1-3 mm was not routinely used in this centre before 2005, possibly causing patient  
343 selection. The one-month or earlier follow-up aortic CT was used in 21.9% of cases and it is unlikely  
344 that a significant change in muscle mass or quality would have developed during that time.  
345 Furthermore, the timing of the imaging was not found to be associated with survival in a Cox  
346 regression analysis. The timing and volume of the contrast agent, and the haemodynamic state of the



347 patient may have influenced the density measurements. Densities measured in small patients with  
348 hyperkinetic circulation may be overestimated compared to large patients with slow circulation.  
349 Another likely yet small contributor to selection bias may have been that in rare cases of unstable  
350 patients requiring immediate intervention, the decision to operate was made based solely on  
351 ultrasound without concomitant CT imaging. The strengths of the present study lie in a large and  
352 homogenous patient cohort comprising elective and urgent or emergency cases and patients treated  
353 with open surgery and EVAR, structural collection of data, and a noticeable follow-up time.

354

## 355 **CONCLUSION**

356

357 L2 – L3 PMD and LPMA offer a valuable adjunct to postoperative risk prediction in patients treated  
358 for AAA and they can be reliably and swiftly measured without added costs. At strongest, this means  
359 that for every standard deviation increased from psoas muscle lean value bilaterally at L3 level there  
360 is a 26% decrease in the probability of death during follow-up. In clinical use PMD and LPMA  
361 standardized z-scoring help to perceive prognosis when standard deviation is known.

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364 **CONFLICTS OF INTEREST**

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368

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## LEGENDS FOR ILLUSTRATIONS

**Fig.1** Muscle measurement. Outlining the region of interest (ROI): Psoas (and multifidus) muscles on both sides. Area was measured in mm<sup>2</sup>. RPMA; right psoas muscle area, LPMA; left psoas muscle area, RMMA; right multifidus muscle area, LMMA; left multifidus muscle area.

**Fig.2** Illustration of the measurement used for this study between vertebrae L2 and L3. Estimating gaps between spinal discs on transverse processes from bottom of the more cranial vertebra.







Table 1. Patient demographics and risk factors.

Features	Sample N=301
<b>Demographics</b>	
Age (years)	74.4 ± 9.4
Male (%)	268 (89%)
Height (m)	1.76 ± .08
BMI (kg/m <sup>2</sup> )	26.6 ± 4.4
<b>Risk factors</b>	
Previous intervention	20 (6.6%)
Smoking	71 (23.6%)
CAD	158 (50.8%)
DM	41 (13.6%)
HTA	192 (63.8%)
Dyslipidemia	132 (43.9%)
Pulmonary disease	68 (22.6%)
Stroke or TIA	34 (11.3%)
Creatinine level (μmol/l)	86 ± 83
<b>Procedural variables</b>	
rAAA	23 (7.6%)
OR	81 (26.9%)
EVAR	220 (73.1%)
ASA 2	16 (5.3%)
ASA 3	176 (58.5%)
ASA 4	92 (30.6%)
ASA 5	17 (5.6%)

## Medication

Antiaggregant	148 (49.2%)
Anticoagulant	72 (23.9%)
Oral antidiabetic	26 (8.6%)
Insulin	19 (6.3%)
Beta blocker	179 (59.5%)
Other antihypertensive	184 (61.1%)
Statin	168 (55.8%)
Glucocorticoid	19 (6.3%)

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CAD, Coronary artery disease; DM, Diabetes mellitus; HTA, Hypertensio arterialis; TIA, transient ischaemic attack; rAAA, ruptured abdominal aortic aneurysm; OR, open repair of abdominal aortic aneurysm; EVAR, endovascular repair of abdominal aortic aneurysm; ASA, American Society for Anaesthesiologists classification.

Table 2. Intraclass correlation coefficient (ICC) analysis of CT-measurements.

Variable		ICC <sup>a</sup>	95% CI	ICC <sup>b</sup>	95% CI	P-value
L2						
dx psoas m.	Area	.686	.36-.89	.585	.21-.85	< .001
	HU	.816	.58-.94	.793	.54-.93	< .001
sin psoas m.	Area	.535	.17-.83	.446	.10-.77	.002
	HU	.769	.50-.92	.776	.51-.93	< .001
dx multifidus m.	Area	-.113	-.34-0.29	-.036	-.10-0.14	.758
	HU	.705	.40-.90	.675	.36-.89	< .001
sin multifidus m.	Area	-.117	-.34-0.31	-.051	-.15-0.20	.726
	HU	.690	.37-.89	.698	.39-.90	< .001
L3						
dx psoas m.	Area	.674	.35-.89	.640	.31-.87	< .001
	HU	.765	.49-.92	.778	.52-.93	< .001
sin psoas m.	Area	.720	.42-.91	.676	.35-.89	< .001
	HU	.691	.37-.89	.693	.38-.89	< .001
dx multifidus m.	Area	.175	-.16-0.61	.076	-.06-0.38	.167
	HU	.823	.59-.94	.818	.59-.94	< .001
sin multifidus m.	Area	-.055	-.30-0.39	-.019	-.10-0.19	.595
	HU	.814	.58-.94	.804	.57-.94	< .001
L4						
dx psoas m.	Area	.812	.57-.94	.740	.40-.92	< .001
	HU	-.036	-.29 – 0.41	-.036	-.30 – 0.41	.553
sin psoas m.	Area	.028	-.25-0.48	.027	-.24-0.46	.416
	HU	.772	.50-.93	.786	.52-.93	< .001

dx multifidus m.	Area	.050	-.24-0.50	.046	-.21-0.47	.372
	HU	.811	.57-.94	.801	.56-.94	< .001
sin multifidus m.	Area	.199	-.14-0.62	.185	-.12-0.60	.138
	HU	.843	.63-.95	.849	.65-.95	< .001
<hr/>						
L5						
dx psoas m.	Area	.916	.79-.97	.862	.57-.96	< .001
	HU	.784	.52-.93	.766	.50-.92	< .001
sin psoas m.	Area	.351	-.02-0.73	.350	-.01-0.72	.032
	HU	.798	.55-.94	.811	.57-.94	< .001
dx multifidus m.	Area	.757	.48-.92	.653	.26-.88	< .001
	HU	.719	.42-.91	.736	.44-.91	< .001
sin multifidus m.	Area	.756	.48-.92	.756	.48-.92	< .001
	HU	.716	.41-.90	.719	.42-.91	< .001
<hr/>						
L2-L3 Distance		.599	.25-.86	.588	.25-.85	.001
L3-L4 Distance		.257	-.10-0.66	.268	-.10-0.68	.084
L4-L5 Distance		.310	-.05-0.70	.287	-.04-0.68	.050

<sup>a</sup> Model: Intraclass correlation coefficient (ICC) two-way random consistency.

<sup>b</sup> Model: Intraclass correlation coefficient (ICC) two-way random absolute.

dx, dexter; sin, sinister; HU, Hounsfield unit.

Table 3. The effect of age, gender and BMI on CT-measurements and the actual medians.

	Age			Gender		BMI			Median	SD
	T1	T2	T3	M	F	T1	T2	T3		
	65.1	74.4	82.4			22.9	26.0	31.1		
Distance between L2-L3 (cm)	34.8	34.0	<b>33.6<sup>a</sup></b>	34.5	31.2	34.3	34.3	34.3	34.3	3.2
L2										
dx PMA (cm <sup>2</sup> )	5.8	4.9	<b>4.3<sup>a</sup></b>	5.2	3.0	4.2	4.8	<b>5.6<sup>c</sup></b>	4.9	2.0
dx PMD (HU)	33.5	28.0	<b>24.0<sup>a</sup></b>	30.0	<b>22.0<sup>b</sup></b>	33.0	28.0	29.0	30.0	12.6
dx lean PMA (cm <sup>2</sup> x HU)	187.6	147.4	<b>109.8<sup>a</sup></b>	154.4	68.9	134.3	148.0	158.4	147.8	93.1
sin PMA (cm <sup>2</sup> )	6.0	5.5	<b>4.6<sup>a</sup></b>	5.6	3.6	4.7	5.5	<b>6.0<sup>c</sup></b>	5.5	1.9
sin PMD (HU)	37.0	30.0	<b>31.0<sup>a</sup></b>	32.0	28.0	34.5	30.0	31.0	31.0	11.8
sin lean PMA (cm <sup>2</sup> x HU)	207.6	166.4	<b>147.4<sup>a</sup></b>	182.8	114.2	169.6	166.6	178.4	170.3	93.1
TPMA (cm <sup>2</sup> )	11.7	10.7	<b>8.9<sup>a</sup></b>	10.9	6.9	8.9	10.6	<b>11.6<sup>c</sup></b>	10.6	3.6
TPMD (HU)	34.8	29.0	<b>27.3<sup>a</sup></b>	31.3	28.0	32.8	29.5	29.5	30.5	11.3
Lean TPMA (cm <sup>2</sup> x HU)	388.3	309.2	<b>254.4<sup>a</sup></b>	330.7	<b>451.0<sup>b</sup></b>	294.8	309.5	329.1	314.0	177.1

L3

dx PMA (cm <sup>2</sup> )	9.1	8.0	<b>7.1<sup>a</sup></b>	8.1	5.1	6.9	8.1	<b>9.1<sup>c</sup></b>	7.9	2.6
dx PMD (HU)	37.0	32.0	<b>29.0<sup>a</sup></b>	33.0	<b>28.0<sup>b</sup></b>	34.5	33.0	32.0	33.0	12.0
dx lean PMA (cm <sup>2</sup> x HU)	310.1	242.4	<b>187.8<sup>a</sup></b>	266.2	<b>121.8<sup>b</sup></b>	221.6	257.3	260.0	253.5	138.2
sin PMA (cm <sup>2</sup> )	9.5	8.2	<b>7.6<sup>a</sup></b>	8.6	<b>5.4<sup>b</sup></b>	7.5	8.5	<b>9.5<sup>c</sup></b>	8.3	2.4
sin PMD (HU)	38.0	33.0	<b>32.0<sup>a</sup></b>	35.0	33.0	37.0	34.0	33.0	34.0	11.3
sin lean PMA (cm <sup>2</sup> x HU)	344.5	280.0	<b>225.4<sup>a</sup></b>	301.2	<b>157.7<sup>b</sup></b>	266.6	280.2	301.2	282.0	135.9
TPMA (cm <sup>2</sup> )	18.5	16.3	<b>14.6<sup>a</sup></b>	16.8	<b>11.0<sup>b</sup></b>	14.5	16.5	<b>18.5<sup>c</sup></b>	16.3	4.9
TPMD (HU)	37.3	32.5	<b>29.5<sup>a</sup></b>	33.5	29.0	34.8	32.5	33.0	33.0	10.8
Lean TPMA (cm <sup>2</sup> x HU)	653.4	522.2	<b>414.2<sup>a</sup></b>	556.5	<b>768.3<sup>b</sup></b>	523.3	540.6	548.4	532.1	262.7
Right psoas volume (cm <sup>3</sup> )	26.3	22.2	<b>18.5<sup>a</sup></b>	23.0	<b>12.8<sup>b</sup></b>	19.0	22.5	<b>25.0<sup>c</sup></b>	21.8	8.2
Lean volume (cm <sup>3</sup> x HU)	849.3	701.7	<b>491.5<sup>a</sup></b>	715.4	<b>338.1<sup>b</sup></b>	617.3	706.7	707.8	684.8	402.6
Left psoas volume (cm <sup>3</sup> )	25.9	23.7	<b>20.9<sup>a</sup></b>	24.4	<b>13.7<sup>b</sup></b>	20.5	23.9	<b>26.2<sup>c</sup></b>	23.7	7.8
Lean volume (cm <sup>3</sup> x HU)	933.8	7765.9	<b>622.6<sup>a</sup></b>	824.0	423.9	748.1	760.1	843.8	785.8	398.6
Total psoas volume (cm <sup>3</sup> )	52.0	45.9	<b>40.0<sup>a</sup></b>	47.2	<b>26.9<sup>b</sup></b>	39.7	45.8	<b>50.5<sup>c</sup></b>	45.5	15.6
Lean total volume (cm <sup>3</sup> x HU)	1770.0	1514.4	<b>1141.7<sup>a</sup></b>	1566.9	<b>747.3<sup>b</sup></b>	1428.4	1505.2	1577.0	1495.2	769.0

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Values presented are medians. T, tertile; M, male; F, female; PMA, psoas muscle area; PMD, psoas muscle density; TPMA, total (sin and dx) psoas muscle area; TPMD, total psoas muscle density; HU, density in Hounsfield units; BMI, body mass index; sin, sinister; dx, dexter; SD, standard deviation. Volumes have been calculated between L2 and L3 vertebrae. <sup>a</sup> The oldest tertile has statistically significant difference compared to the youngest tertile ( $P < .05$ , One-way Anova or Kruskal-Wallis test). <sup>b</sup> Females have statistically significant difference compared to males ( $P < .05$ , independent-samples T-test or chi-squared test). <sup>c</sup> The highest tertile has statistically significant difference compared to the lowest tertile ( $P < .05$ , One-way Anova or Kruskal-Wallis test).

Table 4. Multivariable cox regression analysis of overall survival

Variables	Model 1		Model 2		Model 3		Model 4		Model 5		Model 6		Model 7	
	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI
Age	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.05<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.05<sup>c</sup></b>	<b>1.02-1.09</b>	<b>1.05<sup>c</sup></b>	<b>1.02-1.08</b>
rAAA	<b>5.07<sup>c</sup></b>	<b>2.17-11.84</b>	<b>5.04<sup>c</sup></b>	<b>2.15-11.81</b>	<b>5.16<sup>c</sup></b>	<b>2.21-12.01</b>	<b>4.82<sup>c</sup></b>	<b>2.10-11.10</b>	<b>4.91<sup>c</sup></b>	<b>2.14-11.29</b>	<b>4.78<sup>c</sup></b>	<b>2.09-10.92</b>	<b>4.91<sup>c</sup></b>	<b>2.14-11.26</b>
Smoking	1.09	0.62-1.92	1.12	0.64-1.98	1.07	0.61-1.89	1.06	0.60-1.88	1.07	0.61-1.89	1.02	0.58-1.80	1.05	0.60-1.84
Stroke or TIA	1.82	1.00-3.30	<b>1.83<sup>a</sup></b>	<b>1.00-3.34</b>	1.76	0.97-3.19	1.75	0.96-3.17	1.77	0.97-3.22	1.81	0.99-3.28	1.80	0.99-3.26
Creatinine	<b>1.03<sup>c</sup></b>	<b>1.02-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.02-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>
ASA	1.11	0.76-1.61	1.12	0.77-1.62	1.16	0.81-1.67	1.17	0.81-1.68	1.15	0.80-1.66	1.13	0.79-1.63	1.14	0.79-1.64
Medication														
Anticoagulant	1.13	0.71-1.81	1.12	0.70-1.79	1.08	0.68-1.73	1.10	0.69-1.76	1.11	0.70-1.78	1.11	0.70-1.78	1.11	0.70-1.77
Statin	0.67	0.44-1.03	0.67	0.44-1.02	<b>0.66<sup>a</sup></b>	<b>.43-1.00</b>	0.66	0.43-1.00	0.66	0.43-1.02	0.66	0.43-1.01	0.67	0.44-1.02
CT parameter z-score														
<i>L3 sin PMD</i>	<b>0.76<sup>b</sup></b>	<b>0.63-0.93</b>	-	-	-	-	-	-	-	-	-	-	-	-
<i>L3 TPMD</i>	-	-	<b>0.78<sup>a</sup></b>	<b>0.64-0.95</b>	-	-	-	-	-	-	-	-	-	-
<i>L2 dx LPMA</i>	-	-	-	-	<b>0.78<sup>a</sup></b>	<b>0.61-0.99</b>	-	-	-	-	-	-	-	-
<i>L2 LTPMA</i>	-	-	-	-	-	-	<b>0.78<sup>a</sup></b>	<b>0.61-1.00</b>	-	-	-	-	-	-

<i>L3 dx LPMA</i>	-	-	-	-	<b>0.76<sup>a</sup></b>	<b>0.60-0.95</b>	-	-
<i>L3 sin LPMA</i>	-	-	-	-	-	<b>0.75<sup>a</sup></b>	<b>0.59-0.94</b>	-
<i>L3 LTPMA</i>	-	-	-	-	-	-	<b>0.74<sup>a</sup></b>	<b>0.58-0.93</b>

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PMA, psoas muscle area; PMD, psoas muscle density; TPMD, total psoas muscle density; TPMA, total (sin and dx) psoas muscle area; LPMA, lean psoas muscle area; LTPMA, lean total psoas muscle area; rAAA, ruptured abdominal aortic aneurysm; TIA, transient ischaemic attack; ASA, American Society for Anesthesiologists classification; sin, sinister; dx, dexter. Creatinine level and HU-values are transformed to 1/10 values. The effect of area and volume parameters is presented as per cm<sup>2</sup> and cm<sup>3</sup>, respectively. Hazard ratio (HR) estimated from Cox hazard regression model. Confidence interval (CI) of the estimated HR. <sup>a</sup> Indicates significant difference P<.05, <sup>b</sup> P<.01 and <sup>c</sup>P <.001.

# **Psoas muscle area and quality are independent predictors of survival in patients treated for abdominal aortic aneurysms**

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Niko Sillanpää, MD, PhD <sup>d\*</sup>, Niku Oksala, MD, PhD, DSc <sup>a,b,e\*</sup>

<sup>a</sup> Faculty of Medicine and Life Sciences, University of Tampere, FI-33014, Tampere, Finland

<sup>b</sup> Division of Vascular Surgery, Department of Surgery, Tampere University Hospital, PO BOX 2000  
FI-33521 Tampere, Finland

<sup>c</sup> BioMediTech Institute and Faculty of Biomedical Sciences and Engineering, Tampere University of  
Technology, Tampere Finland

<sup>d</sup> Medical Imaging Center, Tampere University Hospital, PO BOX 2000, FI-33521, Tampere, Finland

<sup>e</sup> Finnish Cardiovascular Research Center, Tampere, Finland

\* These authors share senior authorship

Corresponding author: Professor N. Oksala, Faculty of Medicine and Life Sciences, University of  
Tampere, FI-33014, Tampere, Finland. Email address: niku.oksala@professori.fi

Supplementary table 1. Univariable cox regression analysis of overall mortality.

Risk factor	HR	95% CI
<b>Age</b>	<b>1.06<sup>c</sup></b>	<b>1.04-1.09</b>
Gender	1.05	0.56-1.98
Height	1.00	0.97-1.02
BMI	0.97	0.92-1.02
<b>rAAA</b>	<b>3.25</b>	<b>1.76-6.00</b>
Previous operation	1.05	0.43-2.60
<b>Smoking</b>	<b>0.64<sup>a</sup></b>	<b>0.38-1.09</b>
CAD	1.31	0.87-1.97
DM	1.31	0.74-2.31
HTA	0.92	0.61-1.39
Dyslipidemia	0.70	0.46-1.07
Pulmonal disease	0.95	0.58-1.55
<b>Stroke or TIA</b>	<b>1.79<sup>b</sup></b>	<b>1.01-3.18</b>
<b>Creatine level</b>	<b>1.00<sup>c</sup></b>	<b>1.00-1.01</b>
EVAR	1.28	0.79-2.07
<b>ASA</b>	<b>1.70<sup>c</sup></b>	<b>1.26-2.29</b>
Medication		
Antiaggregant	1.08	0.72-1.62
<b>Anticoagulant</b>	<b>1.50<sup>a</sup></b>	<b>0.96-2.34</b>
Oral antidiabetic	0.96	0.45-2.09
Insulin	0.80	0.32-1.96
Beta blocker	1.04	0.69-1.57

Other antihypertensive	1.06	0.70-1.60
<b>Statin</b>	<b>0.61<sup>b</sup></b>	<b>0.41-0.92</b>
Glucocorticoid	1.76	0.85-3.66

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BMI, Body mass index; rAAA, ruptured abdominal aortic aneurysm; CAD, Coronary artery disease; DM, Diabetes mellitus; HTA, Hypertensio arterialis; TIA, transient ischaemic attack; EVAR, Endovascular aortic repair; ASA, American Society for Anaesthesiologists Classification. Hazard ratio (HR) estimated from Cox hazard regression model. Confidence interval (CI) of the estimated HR. Variables demonstrating significant associations with mortality on univariate analysis ( $P < .1$ ) were incorporated into multivariate analysis. <sup>a</sup> indicates significant difference  $P < .1$ , <sup>b</sup> $P < .05$  and <sup>c</sup> $P < .01$ .

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<sup>a</sup> Faculty of Medicine and Life Sciences, University of Tampere, FI-33014, Tampere, Finland

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[niku.oksala@professori.fi](mailto:niku.oksala@professori.fi)

Supplemenatry table 2. Multivariable cox regression analysis of standardized z-scoring

Variables	Model 1		Model 2		Model 3		Model 4		Model 5		Model 6		Model 7	
	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI
Age	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.06<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.05<sup>c</sup></b>	<b>1.03-1.09</b>	<b>1.05<sup>c</sup></b>	<b>1.02-1.09</b>	<b>1.05<sup>c</sup></b>	<b>1.02-1.08</b>
rAAA	<b>5.07<sup>c</sup></b>	<b>2.17-11.84</b>	<b>5.04<sup>c</sup></b>	<b>2.15-11.81</b>	<b>5.16<sup>c</sup></b>	<b>2.21-12.01</b>	<b>4.82<sup>c</sup></b>	<b>2.10-11.10</b>	<b>4.91<sup>c</sup></b>	<b>2.14-11.29</b>	<b>4.78<sup>c</sup></b>	<b>2.09-10.92</b>	<b>4.91<sup>c</sup></b>	<b>2.14-11.26</b>
Smoking	1.09	0.62-1.92	1.12	0.64-1.98	1.07	0.61-1.89	1.06	0.60-1.88	1.07	0.61-1.89	1.02	0.58-1.80	1.05	0.60-1.84
Stroke or TIA	1.82	1.00-3.30	<b>1.83<sup>a</sup></b>	<b>1.00-3.34</b>	1.76	0.97-3.19	1.75	0.96-3.17	1.77	0.97-3.22	1.81	0.99-3.28	1.80	0.99-3.26
Creatinine	<b>1.03<sup>c</sup></b>	<b>1.02-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.02-1.05</b>	<b>1.03<sup>c</sup></b>	<b>1.01-1.05</b>
ASA	1.11	0.76-1.61	1.12	0.77-1.62	1.16	0.81-1.67	1.17	0.81-1.68	1.15	0.80-1.66	1.13	0.79-1.63	1.14	0.79-1.64
Medication														
Anticoagulant	1.13	0.71-1.81	1.12	0.70-1.79	1.08	0.68-1.73	1.10	0.69-1.76	1.11	0.70-1.78	1.11	0.70-1.78	1.11	0.70-1.77
Statin	0.67	0.44-1.03	0.67	0.44-1.02	<b>0.66<sup>a</sup></b>	<b>.43-1.00</b>	0.66	0.43-1.00	0.66	0.43-1.02	0.66	0.43-1.01	0.67	0.44-1.02
CT parameter														
<i>L3 sin PMD</i>	<b>0.79<sup>b</sup></b>	<b>0.66-0.94</b>	-	-	-	-	-	-	-	-	-	-	-	-
<i>L3 TPMD</i>	-	-	<b>0.80<sup>a</sup></b>	<b>0.66-0.96</b>	-	-	-	-	-	-	-	-	-	-
<i>L2 dx LPMA</i>	-	-	-	-	<b>0.97<sup>a</sup></b>	<b>0.95-1.00</b>	-	-	-	-	-	-	-	-
<i>L2 LTPMA</i>	-	-	-	-	-	-	<b>0.99<sup>a</sup></b>	<b>0.97-1.00</b>	-	-	-	-	-	-



<i>L3 dx LPMA</i>	-	-	-	-	<b>0.98<sup>a</sup></b>	<b>0.96-1.00</b>	-	-
<i>L3 sin LPMA</i>	-	-	-	-	-	<b>0.98<sup>a</sup></b>	<b>0.96-1.00</b>	-
<i>L3 LTPMA</i>	-	-	-	-	-	-	<b>0.99<sup>a</sup></b>	<b>0.98-1.00</b>

CT parameter z-score

<i>L3 sin PMD</i>	<b>0.76<sup>b</sup></b>	<b>0.63-0.93</b>	-	-	-	-	-	-
<i>L3 TPMD</i>	-	<b>0.78<sup>a</sup></b>	<b>0.64-0.95</b>	-	-	-	-	-
<i>L2 dx LPMA</i>	-	-	<b>0.78<sup>a</sup></b>	<b>0.61-0.99</b>	-	-	-	-
<i>L2 LTPMA</i>	-	-	-	<b>0.78<sup>a</sup></b>	<b>0.61-1.00</b>	-	-	-
<i>L3 dx LPMA</i>	-	-	-	-	<b>0.76<sup>a</sup></b>	<b>0.60-0.95</b>	-	-
<i>L3 sin LPMA</i>	-	-	-	-	-	<b>0.75<sup>a</sup></b>	<b>0.59-0.94</b>	-
<i>L3 LTPMA</i>	-	-	-	-	-	-	<b>0.74<sup>a</sup></b>	<b>0.58-0.93</b>

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PMA, psoas muscle area; PMD, psoas muscle density; TPMD, total psoas muscle density; TPMA, total (sin and dx) psoas muscle area; LPMA, lean psoas muscle area; LTPMA, lean total psoas muscle area; rAAA, ruptured abdominal aortic aneurysm; TIA, transient ischaemic attack; ASA, American Society for Anesthesiologists classification; sin, sinister; dx, dexter. Creatinine level and HU-values are transformed to 1/10 values. The effect of area and volume

parameters is presented as per  $\text{cm}^2$  and  $\text{cm}^3$ , respectively. Hazard ratio (HR) estimated from Cox hazard regression model. Confidence interval (CI) of the estimated HR. <sup>a</sup> Indicates significant difference  $P < .05$ , <sup>b</sup>  $P < .01$  and <sup>c</sup>  $P < .001$ .

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<sup>a</sup> Faculty of Medicine and Life Sciences, University of Tampere, FI-33014, Tampere, Finland

<sup>b</sup> Division of Vascular Surgery, Department of Surgery, Tampere University Hospital, PO BOX 2000 FI-33521 Tampere, Finland

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Supplementary table 3. Multivariable cox regression analysis of overall mortality.

Variables	Model 1		Model 2		Model 3		Model 4		Model 5		Model 6		Model 7	
	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI	HR	95% CI
Age	<b>1.06<sup>c</sup></b>	1.03-1.09	<b>1.06<sup>c</sup></b>	1.03-1.09	<b>1.06<sup>c</sup></b>	1.03-1.09	<b>1.06<sup>c</sup></b>	1.03-1.09	<b>1.06<sup>c</sup></b>	1.03-1.09	<b>1.06<sup>c</sup></b>	1.03-1.09	<b>1.06<sup>c</sup></b>	1.03-1.09
Gender	0.61	0.31-1.19	0.57	0.29-1.12	<b>0.47<sup>a</sup></b>	0.23-0.95	<b>0.49<sup>a</sup></b>	0.24-0.98	<b>0.48<sup>a</sup></b>	0.24-0.96	<b>0.43<sup>b</sup></b>	0.21-0.88	<b>0.44<sup>a</sup></b>	0.22-0.89
BMI	0.98	0.93-1.03	0.98	0.93-1.04	1.00	0.95-1.05	1.00	0.82-1.05	0.99	0.94-1.05	1.00	0.94-1.05	0.99	0.98-0.99
CT parameter														
<i>L3 sin PMD</i>	<b>0.76<sup>b</sup></b>	0.63-0.91	-	-	-	-	-	-	-	-	-	-	-	-
<i>L3 TPMD</i>	-	-	<b>0.76<sup>b</sup></b>	0.63-0.92	-	-	-	-	-	-	-	-	-	-
<i>L2 dx LPMA</i>	-	-	-	-	<b>0.96<sup>b</sup></b>	0.94-0.99	-	-	-	-	-	-	-	-
<i>L2 LTPMA</i>	-	-	-	-	-	-	<b>0.98<sup>b</sup></b>	0.97-1.00	-	-	-	-	-	-
<i>L3 dx LPMA</i>	-	-	-	-	-	-	-	-	<b>0.97<sup>b</sup></b>	0.96-0.99	-	-	-	-
<i>L3 sin LPMA</i>	-	-	-	-	-	-	-	-	-	-	<b>0.97<sup>c</sup></b>	0.95-0.99	-	-
<i>L3 LTPMA</i>	-	-	-	-	-	-	-	-	-	-	-	-	<b>0.98<sup>c</sup></b>	0.98-0.99

PMA, psoas muscle area; PMD, psoas muscle density; TPMD, total psoas muscle density; TPMA, total (sin and dx) psoas muscle area; LPMA, lean psoas muscle area; LTPMA, lean total psoas muscle area; rAAA, ruptured abdominal aortic aneurysm; TIA, transient ischaemic attack;

ASA, American Society for Anesthesiologists classification; sin, sinister; dx, dexter. Creatinine level and HU-values are transformed to 1/10 values. The effect of area and volume parameters is presented as per  $\text{cm}^2$  and  $\text{cm}^3$ , respectively. Hazard ratio (HR) estimated from Cox hazard regression model. Confidence interval (CI) of the estimated HR. Other covariates included in the model: rAAA, smoking, stroke or TIA, creatinine, ASA, anticoagulant, statin. <sup>a</sup> Indicates significant difference  $P < .05$ , <sup>b</sup> $P < .01$  and <sup>c</sup> $P < .001$ .

