## A cholesterol analog stabilizes the human β<sub>2</sub>-adrenergic receptor nonlinearly with temperature

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### ABSTRACT

In cell membranes, G protein–coupled receptors (GPCRs) mingle with cholesterol, which modulates their assembly, stability, and conformation. Previous studies have shown how cholesterol modulates the structural properties of GPCRs at ambient temperature. Here, we characterized the mechanical, kinetic, and energetic properties of the human  $\beta_2$ -adrenergic receptor ( $\beta_2$ AR) in the presence and absence of the cholesterol analog cholesteryl hemisuccinate (CHS) at room temperature (25°C), physiological temperature (37°C), and human hyperthermia (42°C). We found that CHS stabilized various structural regions of  $\beta_2$ AR differentially, which changed nonlinearly with temperature. Thereby, the strongest effects were observed for structural regions that are important for receptor signaling. Moreover, at 37°C, but not at 25°C or 42°C, CHS caused the  $\beta_2$ AR to increase and stabilize conformational sub-states to adopt to basal activity. These findings indicate that the nonlinear, temperature-dependent action of CHS in modulating the structural properties of this GPCR is optimized for 37°C.

#### INTRODUCTION

G protein-coupled receptors (GPCRs) constitute one of the largest families of human transmembrane proteins (1, 2) that sense extracellular signals and transduce this information into the cell to initiate cellular responses (3, 4). Members of the GPCR family modulate responses to hormones and neurotransmitters, and play crucial roles in vision, smell, taste, the immune response, and inflammation. One of the structurally and functionally best studied GPCRs is the human  $\beta_2$ -adrenergic receptor ( $\beta_2 AR$ ), which serves as a model of the largest class, class A, of the GPCR family (5, 6). Because  $\beta_2AR$  binds to adrenaline in bronchial tissue, promoting smooth muscle relaxation, and to noradrenaline in cardiac tissues, playing a role in heart function and failure, it is a promising therapeutic target (7-9). The  $\beta_2AR$  and other GPCRs co-exist in multiple conformational states of which certain states become more prominent depending on the GPCR assembly, membrane lipid composition, and ligand-binding (10-13). Detailed insight into how GPCRs interact with the membrane environment has been provided by structural models obtained by X-ray crystallography, nuclear magnetic resonance (NMR), cryo-electron microscopy (cryo-EM), native mass spectrometry (MS), and molecular dynamics (MD) simulations (5, 6, 12-19). Based on this progress, we are now starting to understand how the lipid composition of the cellular membrane modulates the functional state of GPCRs (17, 20, 21). Among the lipids of the cell membrane, cholesterol has prominent roles in modulating the functional state and stability of GPCRs (5, 22). However, how and to which extent cholesterol affects the conformational stability of GPCRs remains a topic of investigation.

Cholesterol, a major component of mammalian plasma membranes, ranges in physiological concentration from 10 to 45 mol% depending on the cell type (23-25) and has crucial roles in modulating the structure-function relationship of transmembrane proteins (22, 26). For example, cholesterol and its more water-soluble analog cholesteryl hemisuccinate (CHS) modulate the ligand-binding and functional states of GPCRs in an allosteric manner and increase the stability of GPCRs (27-29). On the other hand, the structure and function of GPCRs are often characterized at nonphysiological temperatures, although the temperature-dependencies of membrane receptor assembly, stability, and function have been observed frequently (27, 30). Thus, which of the structural properties of GPCRs are modulated by cholesterol and CHS, and how this modulation depends on the physiologically relevant temperature remain to be understood.

High-resolution structures of several GPCRs have revealed cholesterol bound to the receptors (*5*, *27*, *31*, *32*). X-ray structures of  $\beta_2AR$  show cholesterol-binding sites between transmembrane  $\alpha$ -helices TMH1, TMH2, TMH3, and TMH4 (*5*, *27*). Structures of close family members of  $\beta_2AR$  show cholesterol- or CHS-binding sites between TMH2 and TMH4 and between TMH3 and TMH5 for the  $\beta_1$ -adrenergic receptor ( $\beta_1AR$ ), and between TMH2 and TMH3 and between TMH5 and TMH6 for the adenosine A2a receptor ( $A_{2a}AR$ ) (*33*, *34*). Complementary to such static structural models, MD simulations of the  $\beta_2AR$  embedded in lipid membranes support the idea that cholesterol preferentially occupies specific interaction sites of the receptor (*35-37*). Full-atomistic MD simulations spanning time ranges of up to ~100 µs show several high-affinity cholesterol-binding sites of which one is located in a cleft formed at the intracellular surface of TMH1 to TMH4, another at a cleft between TMH5 and TMH6 at the intracellular side, and two closely spaced cholesterol hot spots are located at the extracellular region of TMH5-TMH6-E3-TMH7 (*36*). Although structural models and MD simulations can unveil static and transient interactions of  $\beta_2AR$  and cholesterol, they cannot be used to quantify whether and to what extent cholesterol modulates the

mechanical, kinetic, and energetic properties of the receptor in physiologically relevant time ranges.

Atomic force microscopy (AFM)–based single-molecule force spectroscopy (SMFS) has been introduced to characterize the structural folding and properties of transmembrane proteins, including transporters, ion channels, and GPCRs (*38-42*). When applied to the human  $\beta_2AR$  in the presence of CHS at room temperature (*29*), dynamic SMFS (DFS) has revealed the changes that occur to the mechanical, kinetic, and energetic properties of the  $\beta_2AR$  upon ligand-binding (*38*). However, the understanding of how sensitive such structural properties of GPCRs are to physiological temperature ranges is limited. Here, we applied DFS experiments and atomistic MD simulations to study the role of CHS in modulating the mechanical, kinetic, and energetic properties of  $\beta_2AR$  at room temperature (25°C), at physiological temperature (37°C), and at temperature corresponding to hyperthermia (42°C), which leads to cellular damages in humans (*43, 44*). The insights gained, which defined the structural regions of the  $\beta_2AR$  that are affected by CHS and quantified how their properties depend on temperature, highlight the mechanisms by which sterols optimize the structure-function relationship of the  $\beta_2AR$  to physiological temperature.

#### RESULTS

#### Mapping the mechanical stability of human β<sub>2</sub>AR

To characterize how temperature variations within the physiological range influence the mechanical stability of  $\beta_2AR$ , we reconstituted human  $\beta_2AR$  in 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC) liposomes without or with CHS (DOPC:CHS ratio 10:1 vol:vol) (fig. S1A). The proteoliposomes were adsorbed in buffer to carbon grids or mica for ~ 1 h and imaged by transmission electron microscopy (TEM) or AFM, respectively, where they opened-up as single-layered membrane patches (fig. S1, B to F). To characterize whether the appearance of the membranes changed with temperature, we imaged the samples at 25°C, 37°C, and 42°C by AFM (fig. S2). The membranes and  $\beta_2 AR$  assemblies protruding from the membrane did not change appearance, thus indicating that the lipids did not undergo phase separations and that the  $\beta_2$ ARs did not change their assembly. After imaging the opened-up proteoliposomes by AFM in buffer at room temperature (25°C), the stylus of the AFM cantilever was pushed onto the β<sub>2</sub>AR embedded in a DOPC membrane at ~ 700 pN for 0.5 s (Fig. 1A). In ~ 0.1% of all cases (n > 1,000,000), the mechanical contact promoted the nonspecific attachment of the N-terminal end of  $\beta_2 AR$  to the AFM stylus (29, 38, 45). Subsequently, the AFM cantilever was retracted from the membrane at constant speed. During retraction, the N-terminal end of the receptor was mechanically stretched and the extraction and unfolding of a single  $\beta_2 AR$  was recorded with a force-distance curve (Fig. 1B). As previously reported (29, 38), the force-distance curve showed force peaks extending to distances of  $\sim 80$  nm, which corresponds to the contour length of the fully unfolded and stretched  $\beta_2AR$  polypeptide. The superimposition of 100 force-distance curves, each recorded upon mechanically unfolding a single  $\beta_2 AR$ , revealed the common unfolding pattern of human  $\beta_2 AR$  with eight dominant force peaks (Fig. 1C). Every force peak of the force-distance curve was fitted by the worm-like chain (WLC) model to estimate the contour length of the stepwise unfolded and stretched  $\beta_2AR$  polypeptide (45). The contour lengths of the eight force peaks were then used to localize the beginning and the end of the eight structural segments (S1 to S8) unfolded by  $\beta_2$ AR (Fig. 1D). The mechanical stability of each structural segment, which is typically composed of  $\alpha$ -helices and polypeptide loops (29, 38), is described by the magnitude of the respective force peak (45).

#### CHS protects the β<sub>2</sub>AR from destabilization at 37°C

The superimposition of force-distance curves recorded for  $\beta_2AR$  and other GPCRs is highly reproducible and sensitive to experimental conditions (29, 38, 42, 46). To characterize how temperature influences the stability of the human  $\beta_2AR$ , we used SMFS to record many force-distance curves at 25°C, 37°C, and 42°C (Fig. 2). For  $\beta_2AR$  embedded in DOPC membranes, the force-distance curves revealed considerable temperature dependency (Fig. 2, A to C). The force peaks at contour lengths  $\leq$  135 amino acid residues ( $\leq$  40 nm) were largely reduced in magnitude and distributed randomly upon increasing the temperature from 25°C to 37°C (Fig. 2, A and B). The substantial change of the first force peaks of the force-distance curves suggests the destabilization of the TMHs and polypeptide loops of the N-terminal half of the  $\beta_2AR$  (Fig. 1D). Upon further increasing the temperature to 42°C, all force peaks had reduced magnitude and were distributed randomly, thus indicating that the entire secondary structure of  $\beta_2AR$  was destabilized (Fig. 2, G to I). These results show that human  $\beta_2AR$  embedded in DOPC membranes destabilizes considerably at 37°C and higher temperatures.

Next, we characterized the temperature-dependent stability of human  $\beta_2AR$  embedded in DOPC membranes supplemented with the cholesterol analog CHS (Fig. 2, D to I). Force-distance curves recorded at 25°C for  $\beta_2AR$  in DOPC:CHS resembled those recorded in DOPC, thus indicating that CHS had little effect on the number and position of the unfolding force peaks. (Fig. 2G). The observation that the unfolding force peaks remained unchanged in position suggests that the  $\beta_2AR$  stabilizes the same structural segments and thus exposes the same native fold in DOPC and DOPC:CHS membranes (*29*). However, the magnitude of the unfolding force peaks was slightly greater in the presence of CHS, which suggests that the mechanical stability of the  $\beta_2AR$  was

increased (Fig. 2, A and D, and fig. S3). At 37°C, the SMFS spectrum recorded in DOPC:CHS showed patterns very similar to those recorded at 25°C, thus revealing no considerable changes of  $\beta_2AR$  (Fig. 2, D and E). This finding indicates that the structural stability of  $\beta_2AR$  embedded in DOPC:CHS remains largely unaffected by increasing the temperature from 25°C to 37°C. Comparing the substantial change in force peaks assigned to the N-terminal region of  $\beta_2AR$  in DOPC with the force peaks detected for  $\beta_2AR$  in DOPC:CHS at 25°C (Fig. 2G) and 37°C (Fig. 2H) suggests that CHS protects this structural region against thermal destabilization.

Further increasing the temperature to 42°C changed the force-distance curves recorded for  $\beta_2AR$  in DOPC:CHS in a similar way as was observed for  $\beta_2AR$  in DOPC at 42°C (Fig. 2, C and F). In particular, the eight force peaks had reduced magnitudes and were distributed randomly, as was also indicated in the probability histogram of the force peaks (Fig. 21). We can thus conclude that the presence of CHS in the phospholipid membrane moderately increases the mechanical stability of  $\beta_2AR$  at 25°C and protects the  $\beta_2AR$  from partially destabilizing at 37°C. However, CHS could not protect the  $\beta_2AR$  from destabilizing at 42°C. This thermal destabilization particularly affected the N-terminal structural region of  $\beta_2AR$ , which contains TMH1, TMH2, TMH3, and TMH4. Because these TMHs represent the consensus cholesterol-binding motif that predicts cholesterol binding for 44% of human class A GPCRs (*27*), these results suggest that the cholesterol analog CHS interacts with and stabilizes this structural region.

#### CHS modulates the free-energy landscape of the β<sub>2</sub>AR nonlinearly with temperature

The unfolding force of proteins depends on the speed (time / loading rate) at which they are mechanically stressed (47, 48). Thus, their mechanical, energetic, and kinetic properties are better described by the concept of a free-energy landscape (47-52). In the absence of any detailed information, the free-energy landscape stabilizing each structural segment of  $\beta_2$ AR against mechanical unfolding is best described by a simple, two-state model having a single unfolding barrier (Fig. 3A) (49, 52). To determine the parameters of the free-energy landscape of every structural segment of  $\beta_2$ AR in DOPC and DOPC:CHS membranes, we measured their unfolding forces as a function of loading rate at 25°C, 37°C, and 42°C by DFS (figs. S3 to S5). The loading-rate–dependent unfolding force of every structural segment of  $\beta_2$ AR was fitted with the Bell-Evans model (49, 52, 53) to reveal their free-energy landscape parameters (Fig. 3), including: (i) the distance between the folded and the transition state  $x_u$ , which describes the conformational flexibility (or variability) needed to adopt conformational substates; (ii) the transition rate  $k_0$  or lifetime  $1/k_0$ ; (iii) the stabilizing free-energy barrier  $\Delta G$ ; and (iv) the free-energy landscape roughness  $\varepsilon$  describing the energetic stability of conformational substates.

# Cholesterol increases the conformational flexibility of the $\beta_2$ AR at physiological temperature At 25°C, the distance of the transition state $x_u$ of each structural segment of $\beta_2$ AR showed small differences in the absence and presence of CHS (Fig. 3B). In the presence of CHS, the two struc-

tural segments S1 and S2 increased  $x_u$  moderately from 0.12 to 0.25 nm and 0.15 to 0.25 nm, respectively. At 37°C, however, six of eight structural segments had decreased  $x_u$  values in DOPC, whereas S1, S2, S4, S5, and S6 increased their  $x_u$  values substantially in the presence of CHS. Although the remaining segments S3, S7, and S8 also showed a tendency to increase their  $x_u$  values in CHS, the increase was not statistically significant. Markedly, the  $x_u$  values from the structural segments S1, S2, S5, and S6 ranged from 0.15 to 0.21 nm in DOPC and from 0.49 to 1.01 nm in DOPC:CHS. The biggest difference was observed for segments S1 and S5, which, in the presence of CHS, increased  $x_u \sim$ six-fold to 1.01 and 0.9 nm, respectively. This observation shows that in the presence of CHS at 37°C, five of eight structural segments of  $\beta_2$ AR increased their transition state  $x_u$  and thus their conformational flexibility (Fig. 3B and fig. S4). Upon further increasing the temperature to 42°C, the structural segments had substantially decreased  $x_u$  values ( $\leq 0.2$  nm), which was independent of the presence of CHS. At 42°C, no significant differences in  $x_u$  values were observed among the structural segments in DOPC and DOPC:CHS.

Cholesterol modulates the functional states of various GPCRs (21, 54, 55), whereas the depletion of cholesterol from the membrane of neonatal cardiac myocytes alters the signaling behavior of endogenous β<sub>2</sub>AR (56). NMR and double-electron resonance studies revealed substantial conformational heterogeneity of the  $\beta_2$ AR in the apo state (10). Such heterogeneity gives rise to conformational substates between which  $\beta_2 AR$  must transition to exhibit basal activity (10). Our results show that in the absence of CHS, the  $\beta_2$ AR is exposed to a narrowed conformational space, which implies that the receptor cannot adopt all of the conformational substates available to the  $\beta_2 AR$ exposed to cholesterol. Such a reduction in the multi-state free-energy landscapes was previously predicted to illustrate how GPCRs lose function (51). The observed structural flexibility of segments S1, S2, S5, and S6 in the presence of CHS at 37°C may be interpreted in terms of their relevance for the  $\beta_2AR$  structure-function relationship. For example, the segments S5 and S6 stabilize TM5 and TM6, and  $\beta_2AR$  transiting from the inactive to the active state shows large structural outward movements of TMH6 and TMH5, whereas TMH5 extends its  $\alpha$ -helix towards the cytoplasm (57). On the other hand, TMH1, whose properties are described by segments S1 and S2, is a part of binding pocket for allosteric ligands, which modulate the activity of neurotransmitters and hormones (58). Our results thus suggest that cholesterol assists  $\beta_2 AR$  in maintaining a wide conformational space at 37°C, as is required for receptor function (51).

#### Cholesterol increases the lifetime of the $\beta_2 AR$

At 25°C in DOPC, the first three N-terminal structural segments S1, S2, and S3 showed transition rates  $k_0$  ranging from 1.6 to 7.2 s<sup>-1</sup>. They hence exposed considerably lower kinetic stabilities compared to segments S4 to S8, whose transition rates ranged from  $10^{-4}$  to  $10^{-1}$  s<sup>-1</sup> (Fig. 3C). In DOPC:CHS, the kinetic stability of all structural segments exhibited  $k_0$  values ranging from  $10^{-4}$ to  $10^{-1}$  s<sup>-1</sup>, thus indicating that the presence of CHS increased the kinetic stability of structural segments S1, S2, and S3 of  $\beta_2$ AR. At 37°C, most structural segments of  $\beta_2$ AR embedded in DOPC exhibited substantial increases in their  $k_0$  values, with structural segments S2, S3, S4, and S5 showing the highest values. This result indicates that the  $\beta_2 AR$  in DOPC has reduced kinetic stability at 37°C compared to that at 25°C. In the presence of CHS, however, the transition rates of all structural segments remained considerably low, ranging from  $10^{-11}$  to  $10^{-1}$  s<sup>-1</sup>, which indicates that CHS kinetically stabilized the  $\beta_2$ AR. The highest kinetic stabilization was observed for segments S1, S2, S5, and S6. At 42°C, all structural regions of the receptor exhibited substantial increases in their transition rates regardless of whether the receptor was embedded in DOPC or DOPC:CHS. Together, the results show that CHS kinetically stabilizes  $\beta_2 AR$  at 25°C and protects the receptor from kinetic destabilization at 37°C. However, this stabilizing effect of CHS is lost at 42°C.

The observation that the transition rates of the structural segments of  $\beta_2AR$  increase with temperature is similar to what has been described for bacteriorhodopsin (*59*). Because  $\beta_2AR$  shows structural homologies to bacteriorhodopsin and class A GPCRs, the results suggest that increasing the temperature within the physiological range can kinetically destabilize GPCRs. Although this effect may not hold for the structurally and functionally thermostable transmembrane protein bacteriorhodopsin (60), it is obviously prominent for the structure-function relationship of GPCRs, which are sensitive to much smaller temperature variations (28, 30, 61). For example, the melting temperature of the apelin receptor (APJ), a class A GPCR, lies at ~43°C in the absence of CHS (30). In addition, isothermal denaturation assays in the presence of the strong denaturant GnHCl revealed an 8-fold increased stability of  $\beta_2AR$  at 35°C in the presence of CHS (27). Our finding that CHS kinetically stabilizes the  $\beta_2AR$  structure is in general agreement with such findings. However, our results indicate that the action of CHS on  $\beta_2AR$  is likely tailored to the physiological temperature of 37°C. In particular, the properties of individual structural segments of  $\beta_2AR$  embedded in CHS-containing membranes change nonlinearly with temperature.

#### Cholesterol increases the energetic stability of the $\beta_2 AR$

The free-energy barriers stabilizing individual structural segments of  $\beta_2AR$  at 25°C ranged from 16.4 to 26.0  $k_BT$  in DOPC and from 19.0 to 26.6  $k_BT$  in DOPC:CHS (Fig. 3D). At room temperature, the presence of CHS had no considerable effect in energetically stabilizing the structural regions of  $\beta_2AR$ . However, at 37°C, the free-energy barriers of most of the structural segments were reduced in DOPC, ranging from 16.9 to 19.9  $k_BT$ , whereas they increased in DOPC:CHS to values ranging from 19.0 to 41.7  $k_BT$ . In particular, the energetic stability of segments S1, S2, S5, and S6 increased considerably. At 42°C, the stabilizing effect of CHS was lost and the free-energy barriers were reduced to values ranging from 16.0 to 17.8  $k_BT$  in both DOPC and DOPC:CHS, which supports our initial observation that  $\beta_2AR$  became mechanically destabilized at 42°C (Fig. 2). In summary, these results show that CHS had no substantial effect in energetically stabilizing

 $\beta_2$ AR at 25°C and 42°C. However, CHS stabilized the receptor at 37°C. One may thus speculate that the functional impairment of  $\beta_2$ AR in the absence of cholesterol (*54, 56, 62*) may be due to the energetic destabilization of its structure.

#### Free-energy landscape roughness of the β<sub>2</sub>AR structure

Using the free-energy landscape parameters approximated at 25°C and 37°C, we calculated the free-energy landscape roughness of each structural segment,  $\varepsilon$ , stabilizing  $\beta_2$ AR (Materials and Methods, Eq. 3) in the absence and presence of CHS (Table 1). This roughness is frequently used to describe the local minima of the free-energy landscape, which trap smaller conformational substates of protein structures (Fig. 3a). Thereby rougher free-energy landscapes suggest these smaller conformational substates to expose higher energetic stabilities (*59*). The roughness of most structural segments in the absence and presence of CHS ranged from 3.4 to 5.6  $k_{\rm B}T$ . However, in the presence of CHS, the structural segments S2 and S4 showed a rougher (difference > 1  $k_{\rm B}T$ ) free-energy landscape of 4.6 vs 3.4  $k_{\rm B}T$  and 5.6 vs 4.5  $k_{\rm B}T$ , respectively.

The roughness of the free-energy landscape stabilizing the structural segments of  $\beta_2 AR$  (~ 3 to  $6 k_B T$ ) was similar to that reported for segments of bacteriorhodopsin (~ 4 to  $6 k_B T$ ) (59). In the presence of CHS, the  $\beta_2 AR$  segments S2 and S4, which represent the cytoplasmic end of TMH1, cytoplasmic loop C1, TMH2, and extracellular loop E1, exhibited substantial increases in their free-energy landscape roughness. This increase in roughness suggests that CHS energetically stabilizes the conformational substates of segments S2 and S4. This structural region of  $\beta_2 AR$ , which is part of the consensus cholesterol-binding motif of human class A GPCRs, increases the packing constrains of GPCRs upon binding cholesterol (27). Similarly, TMH2 together with TMH4

increase helical packing in the presence of cholesterol, which serves as a bridge between both TMHs (27). Moreover, because TMH4 is considered to have the weakest fold in  $\beta_2$ AR (27), it can be assumed that the cholesterol bridging TMH2 and TMH4 contributes to the overall stabilization of  $\beta_2$ AR (Fig. 3).

#### MD simulations show segment-dependent interactions of CHS with the $\beta_2 AR$

In our SMFS experiments, the mechanical unfolding of a single  $\beta_2$ AR takes from ~13 ms to ~265 ms depending on the cantilever speed. Although currently available computing resources in national supercomputing centers are exceptional, they do not enable us to atomistically simulate complex systems such as those studied here over the course of several ms. This implies that simulating the unfolding processes observed experimentally by SMFS is not possible unless one simulates the process at an accelerated speed, which may cause artifactual results because highly accelerated speeds unfold proteins far from thermal equilibrium (63). Given this point, we decided not to use atomistic simulations to explore the unfolding process itself. Instead, we used multimicrosecond simulations to gain insight into the molecular-scale mechanisms by which CHS affects the thermal stability and conformations of  $\beta_2$ AR. Such simulations can capture the spontaneous interaction events (associations and dissociations) of CHS and  $\beta_2AR$ , which enabled us to interpret the CHS-induced effects observed in our SMFS experiments. We thus performed multimicrosecond atomistic MD simulations of  $\beta_2 AR$  embedded in DOPC and DOPC:CHS membranes (fig. S6) and calculated the time-correlation functions for the interaction of CHS with the structural segments (figs. S7).

The MD simulation models accounted for seven of the structural segments (S1 to S7) of  $\beta_2AR$ , because the C-terminal end, which in our experiments is described as segment S8, has structurally not been solved (*27*, *36*). The volumetric maps showed CHS to preferentially interact with  $\beta_2AR$  at specific sites located at well-defined structural segments (Fig. 4A). In particular, CHS strongly interacted with structural segment S6, which consists of the intracellular parts of TMH5 and TMH6, and of their connecting loop C3. Note that structural segment S6 matches the position of the cholesterol hot spot IC2 as predicted by our previous simulations (*36*). There is also a high density of CHS observed between two structural segments S1 and S4, which overlaps with the low-affinity interaction site EC3 that was predicted for cholesterol (*36*). In addition, CHS also interacts with structural segment S7 and, to some extent, with structural segment S5, which confirms our previous work that the EC1 interaction site of cholesterol lies at S7 and partly at S5 (*36*).

The interaction times of CHS with  $\beta_2$ AR depend on the structural segment (Table 2 and fig. S7). In particular, the interaction time of CHS was greatest for segments S1, S4, S5, S6, and S7, which correlates with specific CHS interaction sites revealed by volumetric maps of the CHS density (Fig. 4A). Moreover, the interaction energies revealed strong interactions of CHS with the structural segments S1, S4, S5, S6, and S7 of  $\beta_2$ AR (Fig. 4B). These pronounced interactions of CHS with certain structural segments of the receptor may explain why in our SMFS experiments we observed them to be mechanically, kinetically, and energetically stabilized. One exception was segment S2, for which the MD simulations could not explain the experimentally observed stabilization by CHS. We hence speculate that segment S2 may be stabilized by indirect effects of cholesterol on the lipid bilayer properties, such as the modulation of the mechanical properties of the

membrane. Together, the MD simulations suggest how membrane-embedded CHS may interact preferentially with certain functionally important regions of  $\beta_2$ AR.

To learn about the conformational space explored by  $\beta_2AR$ , we performed a principal component analysis (PCA) of the fluctuations of each structural segment for each given temperature (fig. S8 and Fig. 4C). The spread of the fluctuations was calculated by the two major principal components, PC1 and PC2, in the membrane plane. At 25°C,  $\beta_2AR$  exhibits similar structural flexibilities in the presence and absence of CHS. Similarly, at 42°C, CHS does not affect the structural flexibility of  $\beta_2AR$  significantly. However, at 37°C, the presence of CHS increases the structural flexibility of segment S6, and partially also segments S5 and S7, which supports our experimental findings.

#### General overview of temperature-dependent structural properties of $\beta_2 AR$

To provide a general overview of the temperature-dependent  $\beta_2AR$  stabilization by CHS, the structural properties of  $\beta_2AR$  quantified *via* SMFS in the presence and in the absence of CHS (Fig. 3) were mapped onto the  $\beta_2AR$  structure (Fig. 5). The conformational variability, kinetic and energetic stability detected at 25°C, 37°C and 42°C bring our above described findings together, which will be to discussed in the following chapter.

#### DISCUSSION

Upon increasing temperature in the absence of CHS, the experimentally determined unfolding pattern of  $\beta_2AR$  reduced force and became noisy (Fig. 2). Both effects describe the destabilization of various structural regions of  $\beta_2AR$ . At 37°C, mostly the structural segments of the N-terminal region of  $\beta_2AR$  (TMH1 to TMH5) were destabilized and exhibited low kinetic stabilities (Fig. 5).

In the presence of CHS, this structural region of  $\beta_2AR$ , which contains the consensus cholesterolbinding motif of human class A GPCRs (27), was substantially stabilized. However, because cholesterol also modulates the mechanical properties of the membrane, one may speculate that these mechanical properties may modulate the  $\beta_2AR$  stability as well (64). In our SMFS experiments, we characterized the outcomes of both effects, the direct effects resulting from physicochemical interactions and the indirect effects resulting from the mechanical properties of the lipid membrane on the stability of the  $\beta_2AR$ .

In the absence of CHS, the conformational flexibility of the structural segments of  $\beta_2AR$  decreased with increasing temperature from 25°C to 37°C and 42°C (Fig. 5). The decreasing flexibility indicates that the number of conformational states of the receptor were reduced, which is consistent with the picture of kinetic and energetic destabilization of  $\beta_2AR$  (Fig. 5, C and D). However, in the presence of CHS, the conformational flexibility of  $\beta_2AR$  increased upon increasing temperature from 25°C to 37°C. Simultaneously, the kinetic and energetic stabilities of the receptor increased. At the further increased temperature of 42°C, all three parameters, the conformational flexibility, kinetic stability, and energetic stabilized receptor in the absence of CHS. Thus, CHS modulates the structural properties of  $\beta_2AR$  specifically at 37°C. At all three temperatures investigated, MD simulations showed similar probability distributions for the interactions of CHS with  $\beta_2AR$  (Fig. 4A). However, CHS interacted with the structural segments S1, S5, S6, and S7 for greater times (Table 2, fig. S7). Overall, the atomistic MD simulations support the experimentally observed nonlinear stabilization of  $\beta_2AR$  by CHS. Our experiments and simulations indicate that CHS stabilizes specific structural regions of human  $\beta_2$ AR. The largest CHS effects on energetic and kinetic stabilization and conformational space were observed for structural regions that are of importance for  $\beta_2AR$  signaling (TMH5, intracellular loop 3, and TMH6) and the binding of allosteric ligands (TMH1, TMH2, TMH6, and TMH7) (58). The stabilization of these structural regions was particularly effective at  $37^{\circ}$ C, which is physiologically the most relevant temperature for  $\beta_2$ AR. At 42°C, the protective function of CHS was lost and the  $\beta_2$ AR became destabilized. Whereas this type of destabilization may not necessarily lead to immediate thermal denaturation of  $\beta_2 AR$ , it most probably affects the structure-function relationship of the receptor. This nonlinearity suggests that our understanding of how CHS modulates the structural properties of a GPCR at 25°C cannot be necessarily projected to describe how CHS modulates the receptor at 37°C or 42°C. More generally, it is essential to characterize the action of cholesterol on GPCRs at physiologically relevant temperatures. Given the structural and functional homology of GPCRs (65), we suggest that our findings about how temperature and cholesterol modulate the structural properties of  $\beta_2AR$  nonlinearly may be generalized to other class A GPCRs.

In the future, the combination of experimental SMFS studies and theoretical MD simulations presented here may be applied to systematically quantify how functionally or disease-related pointmutations modulate the CHS-promoted temperature-dependent (de-)stabilization of specific structural regions of the  $\beta_2$ AR. Hereto, point mutations of the key residues in the consensus cholesterolbinding motif and in functionally important structural regions may represent promising targets to start with.

#### **MATERIALS AND METHODS**

#### β<sub>2</sub>AR subcloning, expression, purification, and reconstitution

Human  $\beta_2$ AR was expressed and purified as described previously (66). Briefly,  $\beta_2$ AR with a truncated C-terminal end (48 aa) and an N-terminal FLAG epitope followed by a tobacco etch virus (TEV) protease cleavage site was expressed in *Spodoptera frugiperda* (Sf9) insect cells for ~48 hours. To facilitate protein expression, we used a C-terminal truncated  $\beta_2$ AR construct, which does not affect  $\beta_2$ AR signaling (*57*). Successful expression of  $\beta_2$ AR was evaluated by immunofluorescence. Cells expressing  $\beta_2$ AR were harvested by centrifugation at 5000g for 15 min and stored at  $-80^{\circ}$ C. To purify  $\beta_2$ AR from Sf9 cells, a three-step purification procedure was used.  $\beta_2$ AR was reconstituted in DOPC:CHS (10:1, vol:vol) or DOPC lipid vesicles as described previously (*66*). Briefly, a lipid: $\beta_2$ AR mixture was mixed with reconstitution buffer and kept on ice for 2 hours. The lipid to protein ratio was 1000:1 (mol:mol). Detergent was removed with a 25 × 0.8 cm Sephadex G-50 (fine) column and reconstitution buffer [100 mM NaCl, 20 mM Hepes (pH 7.5)].

#### SMFS

 $\beta_2$ AR samples were aliquoted and flash-frozen in liquid nitrogen. For each SMFS experiment, a new sample was thawed freshly and used once. Proteoliposomes of  $\beta_2$ AR reconstituted in DOPC or DOPC:CHS (10:1, wt:wt) were adsorbed to the freshly cleaved surface of mica in SMFS buffer solution [300 mM NaCl, 25 mM MgCl<sub>2</sub>, 25 mM Tris (pH 7.0)] for 1 hour. After the adsorption time passed, the samples were washed several times with SMFS buffer to remove weakly attached membrane patches. SMFS was performed at 25°C, 37°C, and 42°C using fully automated AFM (Force Robot 300, JPK Instruments) and a temperature-controlled sample holder (High temperature heating stage, JPK Instruments). Every freshly thawed  $\beta_2AR$  sample was characterized by SMFS for a maximum of 5 hours after preparation and thereafter discarded. Data for different temperatures and lipid compositions were recorded in random order. 60 µm-long silicon nitride cantilevers (A-BioLever, BL-RC150VB, Olympus, Japan) were calibrated in SMFS buffer before and after each SMFS experiment with the equipartition theorem. SMFS was recorded at different speeds of cantilever retraction (300, 600, 900, 1200, 2500, and 5000 nm s<sup>-1</sup>). Data at 2500 and 5000 nm s<sup>-1</sup> were recorded with an external 16-bit data acquisition card (NI PCI-6221, National Instruments).

#### SMFS data analysis

In total ~6 × 10<sup>6</sup> force-distance curves from more than 300 independent SMFS experiments were recorded for this work over the time course of five years. A mechanically fully unfolded and stretched  $\beta_2AR$  extends to distances of 70 to 90 nm (29, 38). Thus, only force-distance curves showing a force peak pattern extending to distances >70 nm were selected for analysis. Consistent with previous results (29, 38), we observed the N-terminal end of the  $\beta_2AR$  to predominantly attach to the AFM stylus compared to the C-terminus (72%, n = 210). For statistical reasons, we hence focused on the analysis of force-distance curves, which recorded the mechanical unfolding of  $\beta_2AR$  from the N-terminal end. At least 100 force-distance curves recording the mechanical unfolding from the N-terminal end were analyzed for each unfolding speed to minimize the standard error of the mean (SEM). Every selected force-distance curve was then fitted by applying the worm-like-chain (WLC) model, with a persistence length of 0.4 nm and a contour length of 0.36 nm per amino acid residue (67). This WLC fit of each unfolding force peak provided the rupture force required to mechanically unfold a structural segment, as well as the contour length (in amino

acid residues) of the unfolded and stretched polypeptide. All contour lengths and rupture forces of all unfolding force peaks were grouped and analyzed for each experimental condition. Each unfolding force peak assigns the beginning and end of a structural segment stabilizing the unfolding  $\beta_2$ AR structure. The eight main force peaks detected were mapped to the secondary structure of  $\beta_2$ AR as described previously (29, 38). To locate the force peaks within or on the opposite side of the lipid membrane relatively to the pulling AFM cantilever, a membrane thickness of ~4 nm, which corresponds to the contour length of an  $\sim 11$  amino acid residue-long polypeptide stretch, has been considered to approximate the total contour length of the unfolded and stretched polypeptide (45, 68, 69). In this so-called "membrane compensation," the contour length of the unfolded and stretched polypeptide such as was estimated by fitting the force peak with the WLC model is extended by the contour length corresponding to the membrane thickness. Furthermore, at the relatively low unfolding forces applied in our study, the highly conserved disulfide bridge between residues  $\text{Cys}^{106}$  and  $\text{Cys}^{191}$  of  $\beta_2 \text{AR}$  remains intact (38). Because the polypeptide stretch held together by the much stronger disulfide bridge did not unfold in our SMFS experiments, it was not accounted to localize the contour length of the unfolded and stretched polypeptide to a structural segment of  $\beta_2 AR$ .

#### Quantifying free-energy landscape parameters

According to the Bell-Evans model (53), the most probable unfolding force  $F^*$  is a function of the loading-rate r:

$$F^* = \frac{k_{\rm B}T}{x_{\rm u}} ln\left(\frac{x_{\rm u}r}{k_{\rm B}Tk_0}\right)$$
 Eq. 1

where  $k_{\rm B}$  is the Boltzmann constant and *T* the absolute temperature. The most probable unfolding force and loading-rate for every force peak (structural segment) at every speed were calculated taking the maximum of the Gaussian fit of the rupture force and loading-rate distributions. Applying Eq. 1, we then calculated  $x_{\rm u}$  and  $k_0$  for each structural segment depending on the lipid composition and temperature. The height of the free-energy barrier  $\Delta G^{\ddagger}$  was calculated by applying Eq. 2:

$$\Delta G^{\ddagger} = -k_{\rm B} T ln(\tau_{\rm A} k_0)$$
 Eq. 2

Using the DFS parameters, we applied Eq. 3 to quantify the average roughness  $\varepsilon$  of the free-energy landscape in the presence and absence of CHS:

$$\varepsilon^{2} \approx \frac{x_{u}(T_{2})k_{B}T_{2}x_{u}(T_{1})k_{B}T_{1}}{x_{u}(T_{2})k_{B}T_{2}-x_{u}(T_{1})k_{B}T_{1}} \left[ \Delta G_{u} * \left( \frac{1}{x_{u}(T_{1})} - \frac{1}{x_{u}(T_{2})} \right) + \frac{k_{B}T_{1}}{x_{u}(T_{1})} ln \left( \frac{r_{f}(T_{1})x_{u}(T_{1})}{k_{0}(T_{1})k_{B}T_{1}} \right) - \frac{k_{B}T_{2}}{x_{u}(T_{2})} ln \left( \frac{r_{f}(T_{2})x_{u}(T_{2})}{k_{0}(T_{2})k_{B}T_{2}} \right) \right]$$
Eq. 3

#### Statistical data analysis

Overall more than 300 independent SMFS experiments were performed to acquire the necessary statistics for each of the six experimental conditions (e.g., temperature and lipid composition). To access the statistical significance of the differences observed in the presence and absence of CHS, the slopes and intercepts of linear DFS fits were compared (figs. S3 to S5). A method equivalent to ANCOVA (70) and implemented in GraphPad Prism was used. Comparison of the slopes was used to access statistical significance for differences in  $x_u$ , and comparison of the intercepts was used to access statistical significance for differences in  $k_0$ . Differences were considered significant

when *P* values approached \*P < 0.1, \*\*P < 0.05 and mean values did not overlap within their SDs for  $x_u$  and  $\Delta G$ , and their SDs after logarithmical transformation for  $k_0$ , because the distribution of  $k_0$  is right-skewed (Fig. 3, B to D).

#### **All-atom MD simulations**

We performed atomistic MD simulations of  $\beta_2AR$  embedded in a DOPC lipid bilayer in the presence and absence of 10 mol% of CHS, at 25°C, 37°C, and 42°C (Fig. 5 and table S1). Systems explored in this work contained one  $\beta_2AR$  placed in a membrane composed of 202 to 338 lipid molecules. All systems were explicitly solvated by water together with counter ions added to achieve electroneutrality with 150 mM NaCl. Each system was first energy-minimized to remove bad contacts. After energy minimization, we simulated the systems for 25 to 50 ns with position restraints on the receptor heavy atoms and then for another 25 to 50 ns with position restraints only on the receptor backbone atoms. Subsequently, all restraints were released, and every system was subjected to 2.5 µs of simulation, with three simulation repeats for DOPC systems, and with six simulation repeats for DOPC:CHS systems (table S1). All simulations were performed with the GROMACS 5.0.4 package (71) using the all-atom OPLS-AA force field (72). Parameters for CHS were as described previously (73). As used previously for DOPC (36), we used torsional and Lennard-Jones parameters for saturated (74) and unsaturated hydrocarbons (73, 75) and the torsional potential for the glycerol backbone and the phospholipid head group (74). Water molecules were modelled with the TIP3P water model, which is compatible with OPLS parameterization (76). All simulations were performed in the isothermal-isobaric (NpT) ensemble. The v-rescale (stochastic velocity rescaling) thermostat (77), with a time constant of 0.1 ps, was used to maintain the simulation temperature. The temperatures of the  $\beta_2AR$ , lipids, and solvent (water and ions) were

controlled independently. The pressure of the systems was maintained at 1 bar with the Parrinello-Rahman barostat (78) with a time constant of 1 ps. A semi-isotropic scheme was used for pressure control. Simulations were performed with a time step of 2.0 fs. To preserve the lengths of covalent hydrogen bonds, the LINCS algorithm (79) was applied. Periodic boundary conditions were applied in all three directions. Van der Waals interactions were treated using the Lennard-Jones potential with a cut-off distance of 1.0 nm. Long-range electrostatic interactions were evaluated with the particle mesh Ewald algorithm (80) using a real space cut-off of 1.0 nm, a  $\beta$ -spline interpolation (order of 6), and a direct sum tolerance of  $10^{-6}$ . The simulation model used was validated in an exhaustive series of >100-µs atomistic simulations (36).

## SUPPLEMENTARY MATERIALS

Supplementary Methods Figs. S1 to S8. Table S1.

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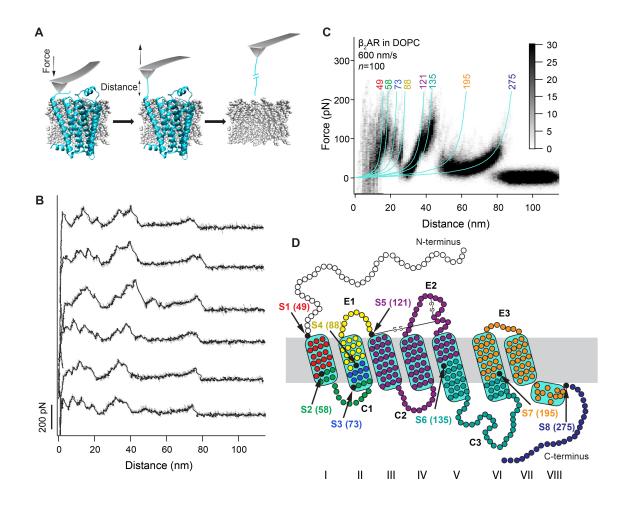


Fig. 1. SMFS analysis of the human  $\beta_2AR$  reveals a common unfolding peak pattern. (A) Schematic representation of the SMFS experiment. The stylus of the AFM cantilever approaches to the surface of  $\beta_2AR$ -containing proteoliposomes until reaching a contact force of 700 pN to nonspecifically attach to the N-terminus of individual receptors (*38*). After 0.5 s, the cantilever is retracted at constant speed and stretches the polypeptide linking the stylus and the  $\beta_2AR$ . At sufficient mechanical force,  $\beta_2AR$  unfolds stepwise until the polypeptide is completely extracted from the membrane. During this process, a force-distance curve is recorded. (**B**) Representative forcedistance curves recorded upon mechanical unfolding of individual  $\beta_2ARs$  from the N-terminal end at 25°C (*38*). (**C**) Superimposition of force-distance curves recorded upon unfolding of  $\beta_2AR$  from a DOPC membrane. The density plot reveals a highly reproducible unfolding fingerprint pattern

of eight force peaks. Each force peak is fitted by the WLC model (gray lines; see Materials Methods) to approximate the contour length of the unfolded and stretched polypeptide. The mean contour lengths given at the top of each WLC curve in amino acids (aa) indicate where a structural segment starts unfolding and the unfolding of the previous structural segment ends. The gray scale bar of the density plot indicates the number of data points superimposed per bin. *n* gives the number of superimposed force-distance curves, which were recorded from more than 10 independent experiments. (**D**) The eight structural segments S1 to S8 mapped to the secondary structure of  $\beta_2$ AR. Helices are numbered with Roman numerals. Extrcellular (E1 to E3) and cytosolic (C1 to C3) loops are labelled. The linearized secondary structure was taken from the study of Zocher *et al.* (*38*) accordingly to tertiary structure model from Protein Data Bank (PDB) ID code 3D4S (*57*).

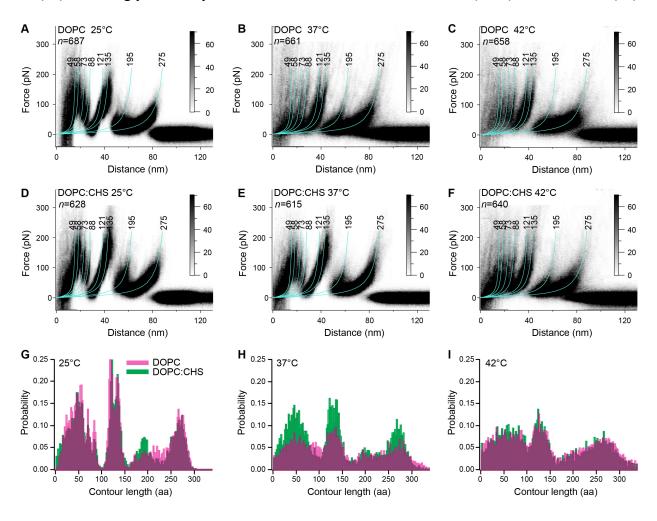


Fig. 2. The unfolding fingerprint pattern of human  $\beta_2AR$  is sensitive to temperature. (A to F) Superimposed force-distance curves recorded upon the unfolding of  $\beta_2AR$  from DOPC (A to C) and DOPC:CHS (D to F) lipid membranes at the indicated temperatures. Every density plot was compiled from force-distance curves recorded at six different unfolding speeds ranging from 300 nm/s to 5000 nm/s (see Materials and Methods). *n* gives the number of force-distance curves superimposed. (**G** to **I**) Contour length histograms mapping the occurrence of unfolding force peaks. The contour length of every unfolding force peak of every force-distance curve was determined as outlined in Fig. 1. The SMFS data were recorded upon the unfolding of  $\beta_2AR$  embedded in DOPC (pink) and DOPC:CHS (green) membranes at 25°C (G), 37°C (H), and 42°C (I). For each experimental condition *n* gives the number of superimposed force-distance curves, which were recorded from more than 60 independent experiments.

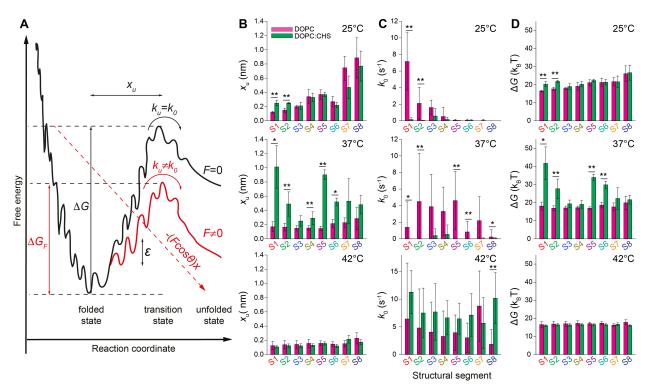
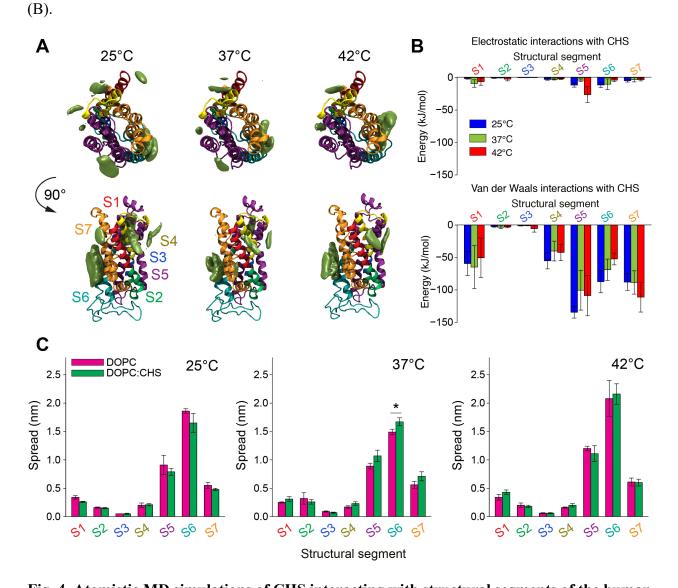


Fig. 3. Unfolding free-energy barrier stabilizing the structural segments of  $\beta_2$ AR. (A) According to the Bell-Evans model (*52, 53*), a natively folded structure resides in a free-energy valley,

which is separated from the unfolded state by a free-energy barrier (black line). Unfolding the structure is initiated by overcoming the transition state of the free-energy barrier.  $x_u$  is the distance between the folded and transition states,  $k_0$  is the transition rate to overcome the free-energy barrier  $\Delta G$  in the absence of an external force (thermal equilibrium), and  $\varepsilon$  is the free-energy landscape roughness. Externally applying a mechanical force F reduces the thermal likelihood of the structure to reach the transition state. The free-energy projection along the reaction coordinate (pulling direction of the externally applied force) is tilted by the applied mechanical energy  $-F(\cos \Theta)x$  (red dashed line), where  $\Theta$  is the angle between reaction coordinate and the externally applied force. This tilt decreases the free-energy barrier height (red line), thereby increasing the probability of the folded structure to overcome the transition state towards unfolding. (B) Distance between the folded and transition state ( $x_u$ ) of the structural segments S1 to S8 of the  $\beta_2$ AR embedded in DOPC and in DOPC-CHS. (C) Transition rates ( $k_0$ ) of the structural segments S1 to S8 of the  $\beta_2$ AR embedded in DOPC and in DOPC-CHS. (D) The free-energy barrier height stabilizing each structural segment of the  $\beta_2AR$  embedded in DOPC and in DOPC-CHS. The values of parameters characterizing the free-energy landscape were obtained from fitting the Bell-Evans model to DFS plots recorded at 25°C, 37°C, and 42°C in the absence (pink) and in the presence (green) of CHS (see Materials and Methods, figs. S3 to S5). The raw data of the SMFS experiments, the number of force-distance curves analyzed and their analysis is given in Figs. 2 and 3. More than 300 independent experiments were performed over the time course of 5 years to acquire the necessary statistics (Materials and Methods). Statistical significance was determined by comparing the slopes and intercepts of linear regressions of the DFS plots in the presence and absence of CHS (figs. S3 to S5) by a method equivalent to ANCOVA (70). Differences were considered significant if Pvalues approached \*P < 0.1 or \*\*P < 0.05 and if experimentally determined values did not overlap



within their SDs (A and C) or their SDs after logarithmical transformation of skewed  $k_0$  distribution

Fig. 4. Atomistic MD simulations of CHS interacting with structural segments of the human  $\beta_2 AR$ . (A) Volumetric maps of the density of CHS (green surface) interacting with human  $\beta_2 AR$  at 25°C, 37°C, and 42°C. At each temperature, the data were averaged from at least six independent trajectories (table S1). The structural segments of  $\beta_2 AR$  are color-coded according to Fig. 1D. (B) Interaction energies resulting from the electrostatic (top) and van der Waals (bottom) interactions of CHS with the indicated structural segments of the human  $\beta_2 AR$  at 25°C, 37°C, and 42°C. Bars and error bars of each structural segment show means  $\pm$  SD (n  $\geq$  3, table S1). (C) Structural

fluctuations of the indicated structural segments of  $\beta_2$ AR projected along two major principle components parallel to the membrane plane. Bars describe the fluctuations of stable structural segments in the absence (pink) and in the presence (green) of CHS. The error (SD) of the spread estimation is <20%. For a description of the PCA used, see the Supplementary Materials. Differences were considered significant if *P* values approached \**P*<0.1 (calculated from a two-tailed t-test) and if the determined values did not overlap within their errors.

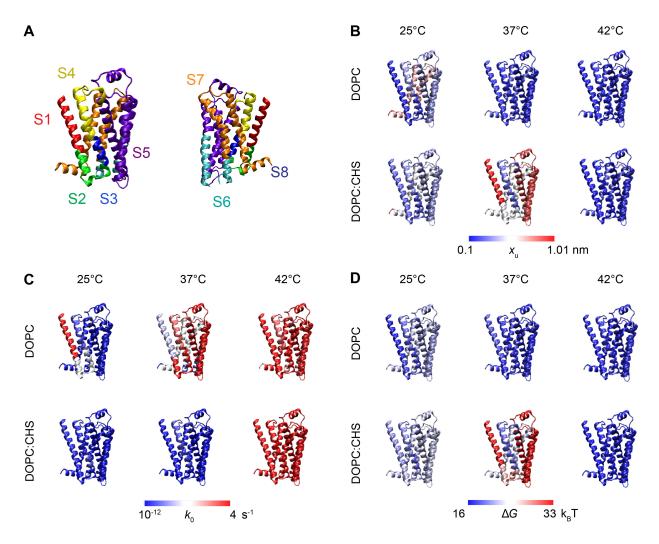


Fig. 5. Temperature-dependent kinetic and energetic properties of human  $\beta_2 AR$  in the presence and absence of CHS. (A) Eight structural segments (taken from Fig. 1) mapped to the structure of human  $\beta_2 AR$  [PDB ID: 3D4S; (57)]. (B) Distance between the folded and transition states,

 $x_{u}$ . (C and D) Transition rate  $k_0$  (C) and height of the free-energy barrier  $\Delta G$  (D) of the structural segments of  $\beta_2AR$ . The individual parameters are explained in Fig. 3 and their values were obtained from SMFS data recorded of  $\beta_2AR$  embedded in DOPC membranes in the absence and presence of CHS at 25°C, 37°C, and 42°C (Fig. 3).

Table 1. Energy landscape roughness  $\varepsilon$  of the structural segments of  $\beta_2 AR$  in the absence and presence of CHS.  $\varepsilon$  values and SD values were calculated by applying Eq. 3 (Materials and Methods) to the DFS data recorded at 25°C and 37°C. Structural segments changing  $\varepsilon > 1 k_B T$  are marked by asterisks.

Structural	DOPC	DOPC:CHS	
segment	$(k_{\rm B}T)$	$(k_{\rm B}T)$	
S1	$3.9 \pm 2.5$	4.5 ± 1.0	
S2*	3.4 ± 11.6	4.6 ± 1.6	
S3	4.6 ± 1.9	$4.0 \pm 6.0$	
S4*	4.5 ± 1.4	5.6 ± 11.1	
85	4.8 ± 1.1	$4.7\pm0.6$	
S6	5.1 ± 5.9	4.5 ± 1.0	
S7	4.8 ± 1.5	4.6 ± 19.6	
S8	5.4 ± 2.9	5.5 ± 4.0	
Mean ± SD	4.6 ± 3.6	$4.8 \pm 5.6$	
of S1 to S8			

Table 2. Interaction times of CHS with structural segments of the  $\beta_2AR$  as revealed from MD simulations. The average interaction times and SD values were calculated from the decay of time-correlation functions (fig. S7) by identifying the times when the time-correlation function was reduced to a value that was either 10 or 1% of the value at time zero. For the analysis shown here, we used data that were averaged over the six simulation repeats and the three simulation temperatures to maximize sampling and thus render the segment-based trend as clearly as possible.

Struc- tural segment	Interaction time (10%) (ns)	Interaction time (1%) (ns)
S1	81.4 ± 21.5	284.5 ± 48.3
S2	$17.7 \pm 10.4$	140.5 ± 65.0
S3	31.4 ± 31.0	231.8 ± 182.7
S4	$111.8 \pm 67.6$	295.2 ± 88.8
S5	$183.8 \pm 52.8$	410.9 ± 58.8
S6	129.3 ± 57.9	406.8 ± 203.1
S7	134.1 ± 66.1	492.8 ± 103.4
Mean ±	98.5 ± 69.3	317.7 ± 157.1
SD of S1		
to S7		

#### **Supplementary Methods**

#### Simulation setup and analysis: B2AR structure

The initial coordinates of the  $\beta_2AR$  (amino acid residues 32 to 342) were taken from our previous work (*36*), in which the structural modifications made for crystallization of the human  $\beta_2AR$  in its inactive state [PDB: 3D4S] (*27*) were reverted back to its pristine sequence. We therefore removed the mutations present in the crystal structure: the E122<sup>3.41</sup>W mutation located in the transmembrane helix TMH3 and the N187<sup>5.26</sup>E mutation located in the extracellular loop E2. Furthermore, because in the crystal structure the residues 231 to 262 of the intracellular loop C3 were substituted with a T4-lysozyme to facilitate experimental structure determination, we removed the T4-lysozyme attached between TMH5 and TMH6 and replaced it with the missing loop C3. The unresolved (and presumably disordered) N-terminal and C-terminal regions were not included in the simulation model. Details of the procedure used to prepare the receptor model for the simulations are discussed previously (*36*). Here, we used the final structure that resulted from this detailed preparation process.

#### Simulation setup and analysis: Embedding β<sub>2</sub>AR in lipid membranes

In the present simulations, we used two different lipid compositions: a single-component DOPC membrane, and a DOPC membrane with 10 mol% CHS (table S1 and fig. S6). The apo-receptor was embedded into a pre-equilibrated (for 100 to 200 ns) lipid membrane in a manner whereby the initial lipid arrangement around the receptor was completely random. For each lipid composition, we prepared three different starting structures with a different organization of lipids around the  $\beta_2AR$ . Each of these six systems was simulated at 25°C, 37°C, and 42°C. In total, we performed 18 simulations, each covering a period of 2.5 µs, with a total simulation length of >45 µs.

## Analyzing the interaction time of CHS with the structural segments (S1 to S7) on the receptor surface

We analysed the binding and unbinding events of each individual CHS molecule with the seven structural segments (S1 to S7) of the  $\beta_2$ AR. CHS was considered to be bound to a segment when the distance of any one of its atoms was  $\leq 0.5$  nm from any atom in the segment. After CHS bound to a structural segment, we determined the probability that CHS at a later time remained bound to the same segment by using the data of all individual binding and unbinding events to compute the (normalized) time-correlation function. The decay of the time-correlation function revealed the average interaction time of CHS binding (fig. S7). The trajectories of all simulation repeats were used for binding analysis.

#### Principal component analysis

Principal component analysis (PCA) is widely used to extract the essential dynamical motions of biomolecules by filtering global and collective (often slow) motions from local and fast motions (81, 82). To perform PCA, we first calculated the covariance matrix C, where the matrix elements  $C_{ij}$  are defined as:

$$C_{ij} = \langle (x_i - \langle x_i \rangle)(x_j - \langle x_j \rangle) \rangle$$

where  $x_i$  and  $x_j$  are the instant coordinates of the i<sup>th</sup> and j<sup>th</sup> atom, and  $\langle x_i \rangle$  and  $\langle x_j \rangle$  are the average coordinates of the respective atoms over the ensemble. By diagonalization and solving the eigenvalue and eigenvectors for the covariance matrix C, we obtained the principal components (PCs). The eigenvectors of these PCs represent the directions of the motions, whereas the corresponding eigenvalues show the magnitudes of the motions along the given directions. Here, we used the g\_covar and g\_anaeig tools from the GROMACS package to perform the PCA analysis over the receptor backbone atoms. We projected our trajectory along the two main PCs (PC1 and PC2) in the membrane plane. An example of such analysis for structural segment S5 at 42°C is shown in fig. S8. Finally, the spread of these projections was calculated as the standard deviation (SD) from the barycenter of the distribution.

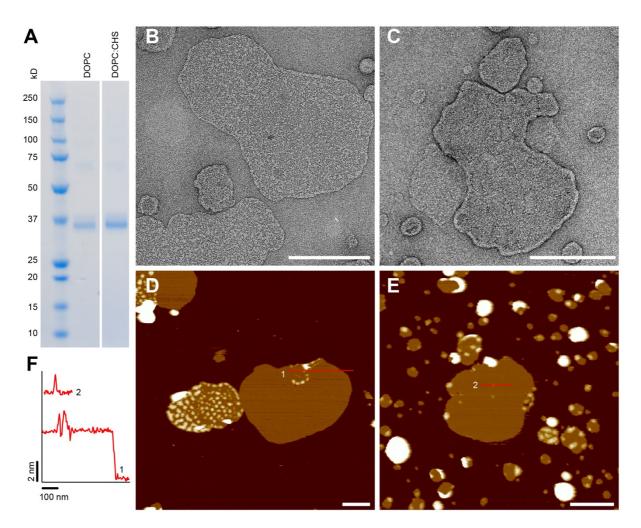


Fig. S1. Human  $\beta_2$ AR reconstituted in DOPC membranes in the presence and absence of CHS. (A) Coomassie blue–stained SDS gel (4 to 12%) of  $\beta_2AR$  reconstituted into DOPC liposomes (second lane) and DOPC:CHS liposomes (9:1, weight:weight, third lane). (B and C) TEM images of β<sub>2</sub>AR reconstituted into DOPC (B) and DOPC:CHS (C) proteoliposomes. For TEM 5 µl proteoliposome solution was pipetted onto a glow-discharged copper grid coated with carbon. After an adsorption time of 1 min, the grid was washed with 4 droplets of milliQ water and subsequently stained with 2% (w/v) uranyl acetate for 10 s, blotting between each step. Grids were imaged using a transmission electron microscope (TEM) with a LaB6 filament operated at 120 kV (Tecnai G2 Spirit BioTWIN, FEI Company, Eindhoven, The Netherlands). Images were recorded by a side-mounted EMSIS MORADA camera. (**D** and **E**) AFM topographs of  $\beta_2$ AR in DOPC (D) and in DOPC:CHS (E) proteoliposomes adsorbed to mica. Upon attachment to mica, most of the proteoliposomes opened and adsorbed as singlelayered membranes. (F) Height profile along the red lines on the AFM topographs (D and E). The membranes protruded  $\sim 5$  to 6 nm above the mica surface and the smaller assemblies of membrane proteins protruded ~1 to 2 nm above the lipid membrane. Topographs were recorded by contact mode AFM in SMFS buffer solution and at room temperature as described previously (45). Scale bars, 200 nm. The full-range color range of the AFM topographs corresponds to vertical scales of 16 nm (D) and 16.5 nm (E). Each experiment shown has been repeated at least 3 times revealing similar results.

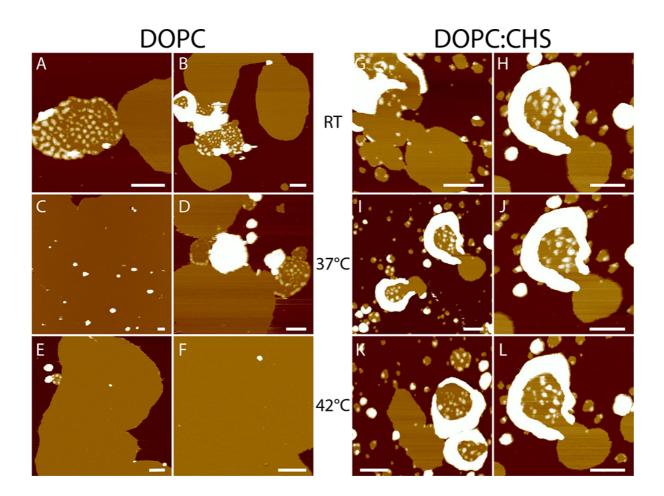


Fig. S2. AFM topographs of human  $\beta_2$ AR reconstituted in DOPC membranes in the presence and absence of CHS and recorded at different temperatures. (A to F) AFM topographs of  $\beta_2$ AR reconstituted in DOPC membranes and imaged at room temperature (25°C), 37°C, and 42°C. (G to L) AFM topographs of  $\beta_2$ AR reconstituted in DOPC:CHS membranes and imaged at room temperature, 37°C, and 42°C. Topographs were recorded by FD-based AFM in SMFS buffer solution (see Materials and Methods). None of the AFM topographs recorded (n > 50) revealed phase separations of the membranes made from DOPC only or made from the lipid mixture (DOPC:CHS). The white dots protruding from the membranes represent single receptors or assemblies of  $\beta_2$ AR. The full-range color ranges of the AFM topographs correspond to vertical scales of 20 nm (A), 19 nm (B), 32 nm (C), 28 nm (D), 20 nm (E), 19 nm (F), 17 nm (G), 18 nm (H), 17 nm (I), 18 nm (J), 19 nm (K), and 18 nm (L). Scale bars, 200 nm. Each experiment shown has been repeated at least 3 times revealing similar results.

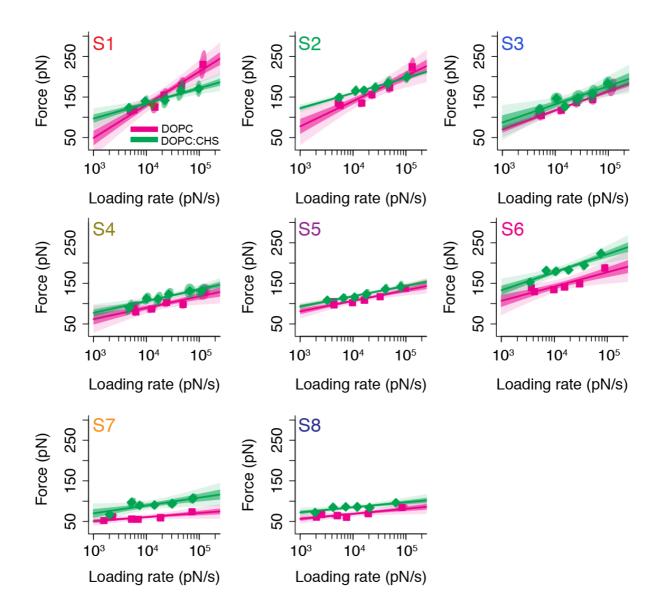


Fig. S3. CHS moderately changes the structural properties of human  $\beta_2AR$  at 25°C. DFS plots of each structural segment (labeled S1 to S8; Fig. 1D) stabilizing  $\beta_2AR$  reconstituted into phospholipid (DOPC) membranes with and without CHS at 25°C. Each DFS plot describes the dynamic behavior of a stable structural segment in the absence (pink) and presence (green) of CHS. Each data point gives the mean unfolding force versus the mean loading rate. Slanted ellipses indicate one standard error. The data points has been extracted from the force-distance curves shown in Fig. 2 (see Materials and Methods). To obtain the unfolding free-energy barrier parameters, the Bell-Evans model (*52*) was fitted (solid lines) to the DFS plots (Materials and Methods; Equation 2). Fitting confidence intervals of one (68%) and two (95%) standard deviations are indicated by dark- and light-colored regions, respectively.

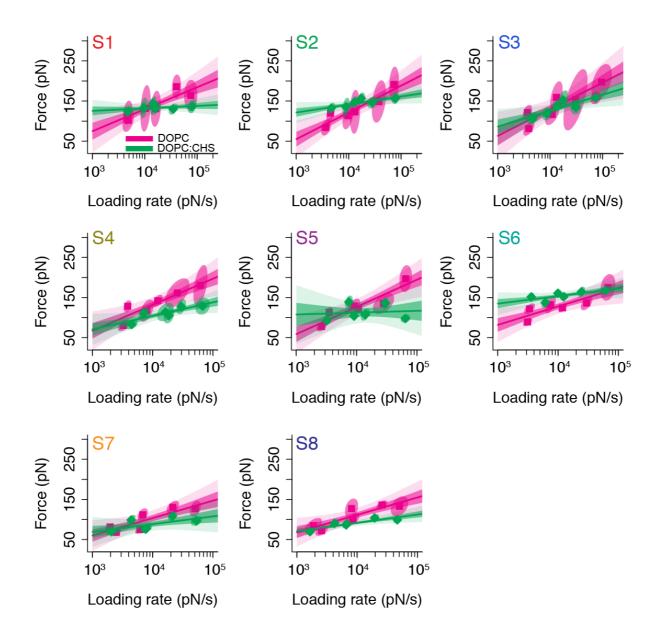


Fig. S4. CHS substantially changes the structural properties of human  $\beta_2AR$  at 37°C. DFS plots of each structural segment (labeled S1 to S8; Fig. 1D) stabilizing  $\beta_2AR$  reconstituted in phospholipid (DOPC) membranes with and without CHS at 37°C. Each DFS plot describes the dynamic behavior of a stable structural segment in the absence (pink) and presence (green) of CHS. Each data point gives the mean unfolding force versus the mean loading rate. Slanted ellipses indicate one standard error. The data points has been extracted from the force-distance curves shown in Fig. 2 (see Materials and Methods).To obtain the unfolding free-energy barrier parameters, the Bell-Evans model (*52*) was fitted (solid lines) to the DFS plots (Materials and Methods; Equation 2). Fitting confidence intervals of one (68%) and two (95%) standard deviations are indicated by dark- and light-colored regions, respectively.

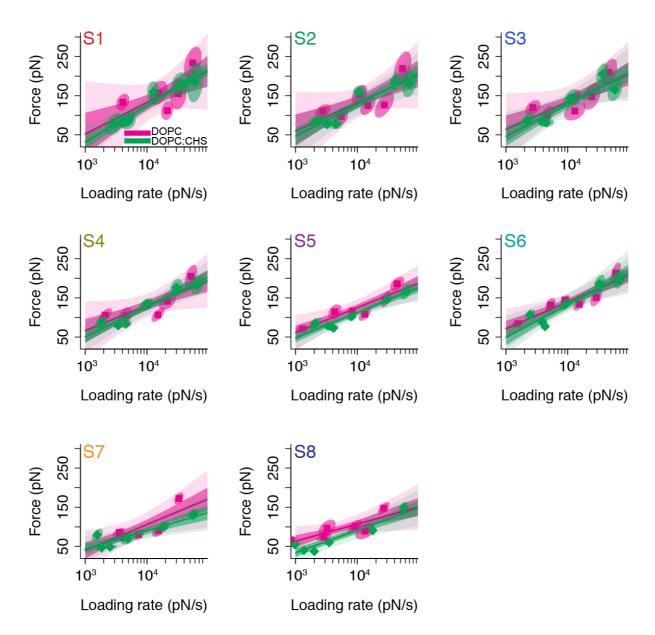


Fig. S5. CHS has little influence on the structural properties of human  $\beta_2AR$  at 42°C. DFS plots of each structural segment (labeled S1 to S8; Fig. 1D) stabilizing  $\beta_2AR$  reconstituted in phospholipid (DOPC) membranes with and without CHS at 42°C. Each DFS plot describes the dynamic behavior of a stable structural segment in the absence (pink) and presence (green) of CHS. Each data point gives the mean unfolding force versus the mean loading rate. Slanted ellipses indicate one standard error. The data points has been extracted from the force-distance curves shown in Fig. 2 (see Materials and Methods).To obtain the unfolding free-energy barrier parameters, the Bell-Evans model (*52*) was fitted (solid lines) to the DFS plots (Materials and Methods; Equation 2). Fitting confidence intervals of one (68%) and two (95%) standard deviations are indicated by dark- and light-colored regions, respectively.

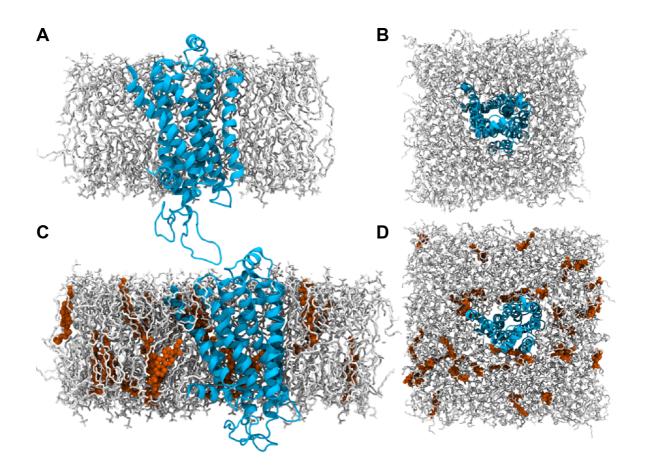


Fig. S6. Atomistic MD simulations of the  $\beta_2$ AR. (A to D) Side (A and C) and top (B and D) views of human  $\beta_2$ AR embedded in DOPC (A and B) and DOPC:CHS (C and D) membranes used in atomistic MD simulations.  $\beta_2$ AR is shown in cartoon form in cyan. DOPC and CHS are colored gray and orange, respectively.

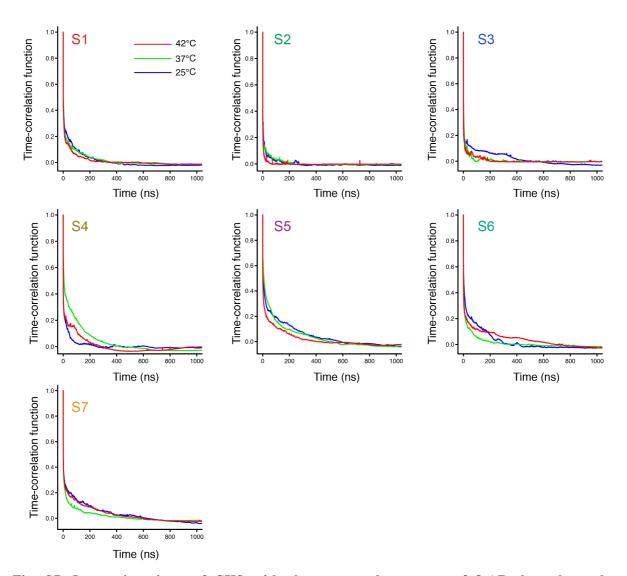


Fig. S7. Interaction times of CHS with the structural segments of  $\beta_2AR$  depend on the temperature. Time-correlation functions describing the interaction time of CHS with the seven structural segments (S1 to S7) of  $\beta_2AR$  at 25°C (blue), 37°C (green), and 42°C (red). Each condition has been simulated at least 3 independent times revealing similar results (see table S1).

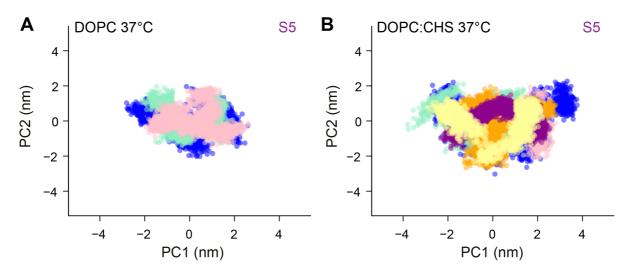


Fig. S8. Structural fluctuations of the structural segment S5 depend on the presence of CHS. (A and B) Projections of the structural fluctuations of the structural segment S5 of  $\beta_2$ AR in DOPC at 37°C without (A) and with (B) CHS. These projections are of simulation trajectories along the first and second principal components (PC1 and PC2). The results of three (A) and six (B) independent simulations (see table S1) are highlighted in different colors.

## Table S1. Systems simulated.

System	Temperature (°C)	Number of repeats	Simulation time of each simulation repeat (µs)
β <sub>2</sub> AR in DOPC	25	3	2.5
membrane	37	3	2.5
	42	3	2.5
$\beta_2 AR$ in DOPC	25	6	2.5
membrane with 10 mol%	37	6	2.5
CHS	42	6	2.5